

Angiogenesis and vascular network remodeling in a growing tumor

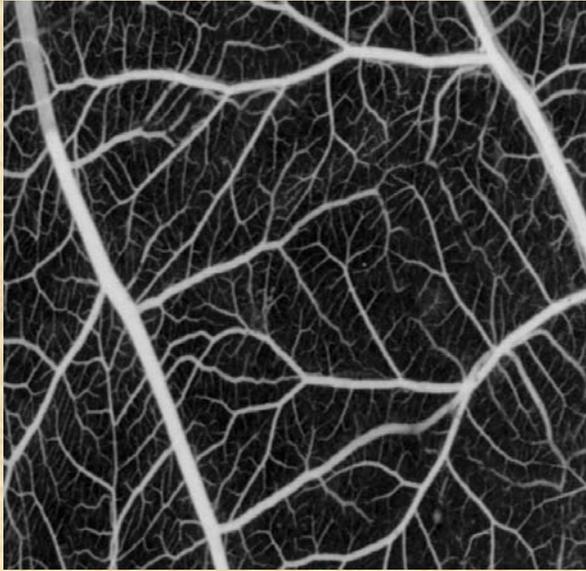


Collaborators

**K. Bartha - Medical Biochemistry,
Semmelweis University for Medicine,
Budapest**

**D.S. Lee, M. Welter, R. Paul
- Theoretical Physics, Saarland University**

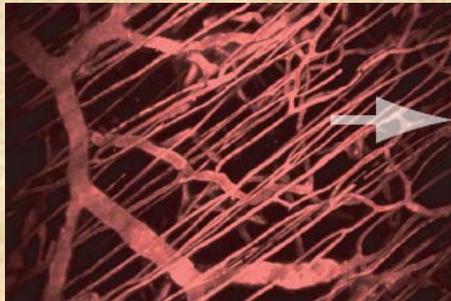
Normal vascularization vs. tumor vessels



Normal capillary network (Oh et al. 1996)



Dilated vessels, brush border effect in the periphery of a melanoma (Steiner et.al.,1992)



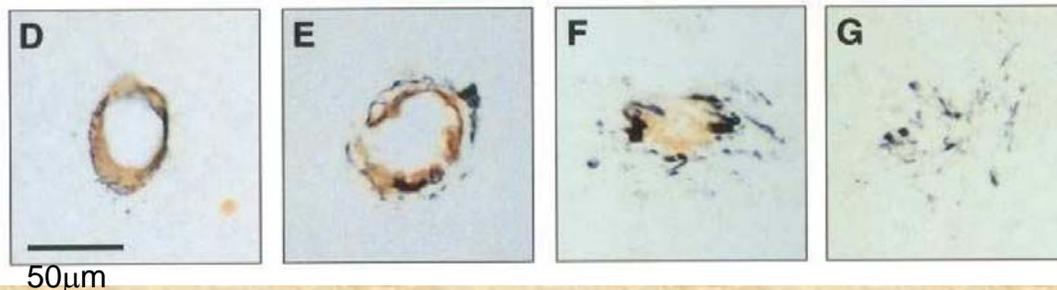
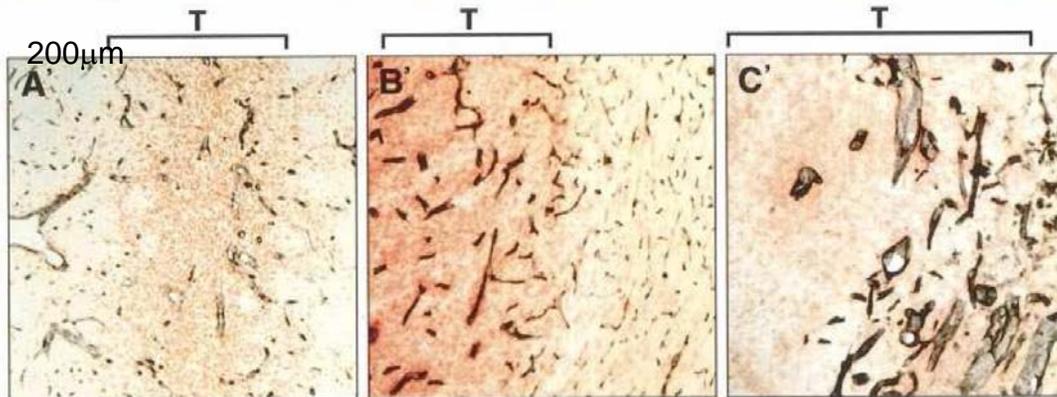
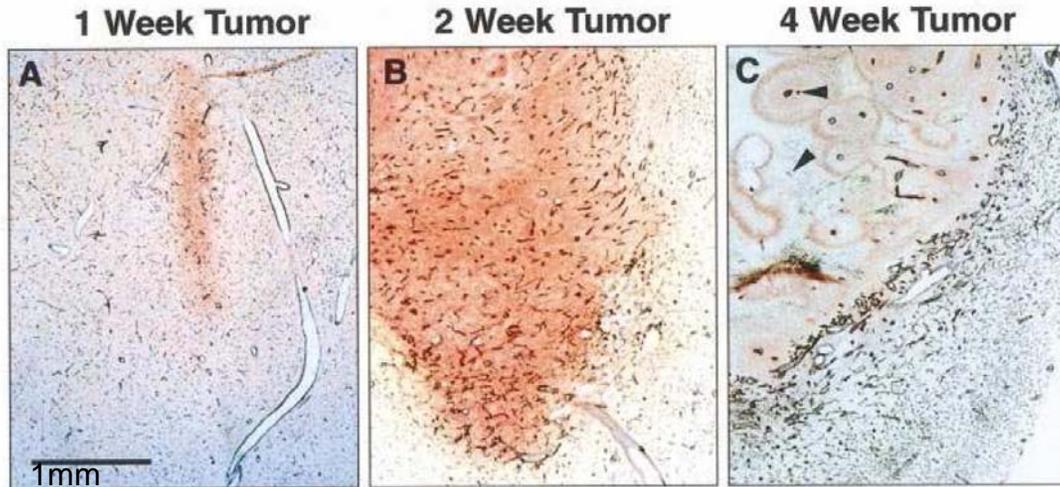
Capillaries in muscle tissue

Progressive vessel regression in growing tumors

Sections from
rat brain tumor

Black:
Vessel-walls

Red:
Tumor cells (TCs)

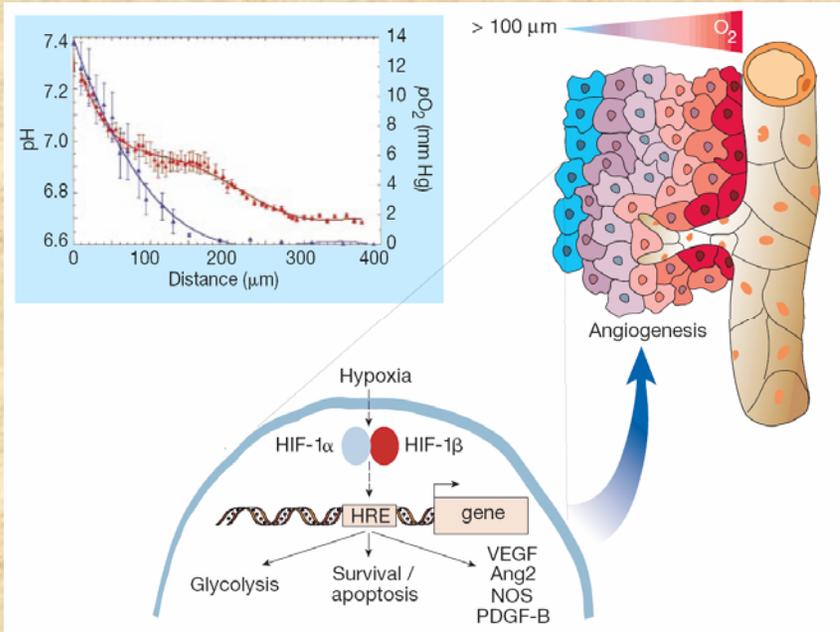


Section through
normal vessel (D),
tumor vessels (E-G)

[from Holash et al.,
Science 284, 1994
(1999)]

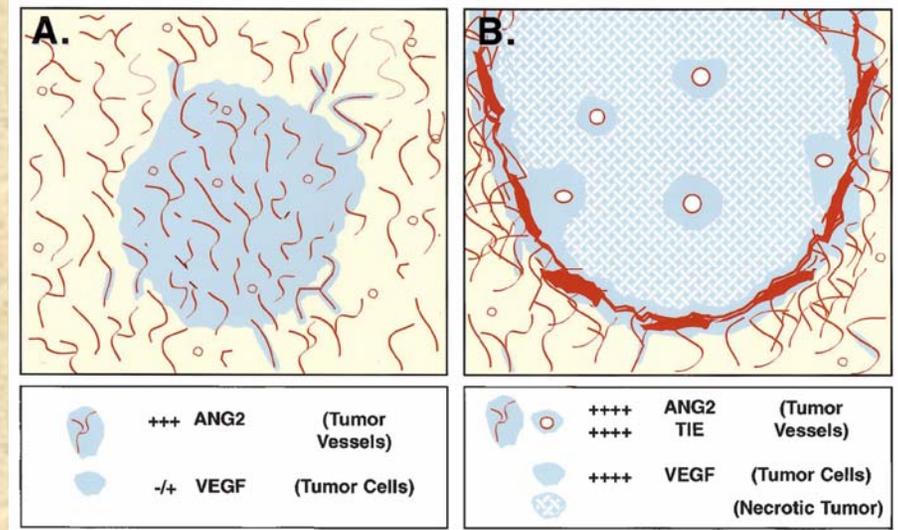
Angiogenesis / Oxygen / HIF / Cooption

Oxygen diffusion range / Hypoxia



[from Carmeliet and Jain, Nature 407, 249 (2000)]

Vessel cooption

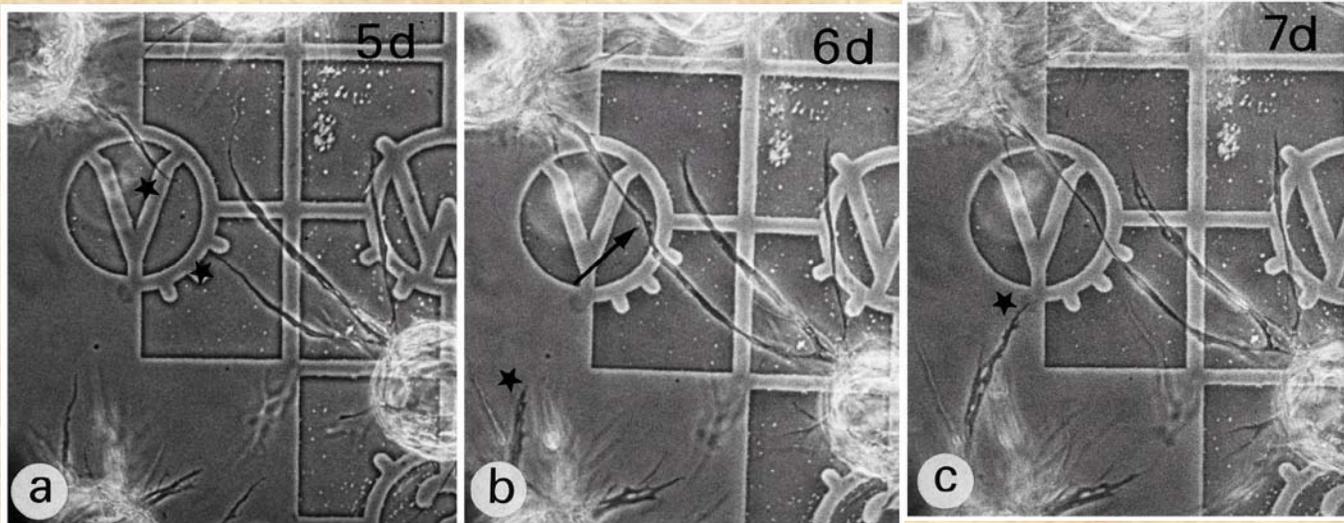


Changes in tumor vasculature during growth. After co-opting host vessels, tumors (gray) initially grow as well as vascularized masses (A). As tumor growth progresses, many of the central tumor vessels regress (B), resulting in massive TC death and necrosis (stippled region). Surviving TCs form cuffs around the few remaining internal vessels.

[from Holash et al., Science 284, 1994 (1999)]

Capillary network remodeling in vitro:

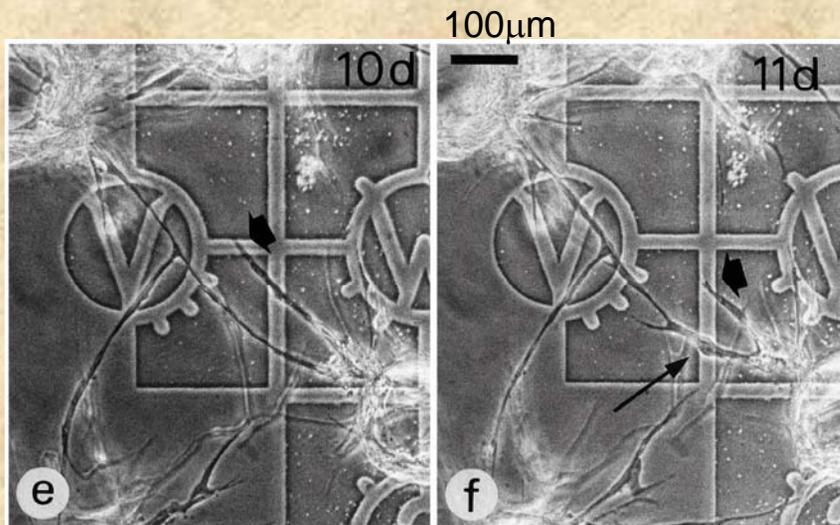
Migration and anastomosis of endothelial cells (EC)



Matrix:
Fibrin gel + bFGF

Microcarriers
coated with ECs

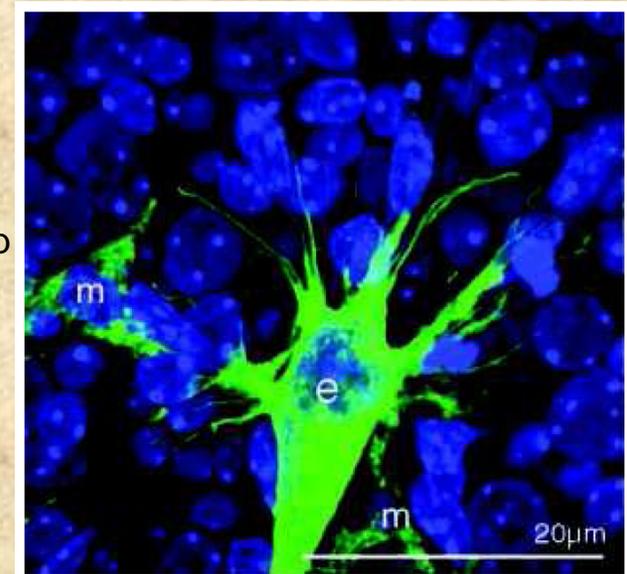
Nehls, Herrmann, Hühnken
Hist. Cell Biol. 109, 319
(1998)



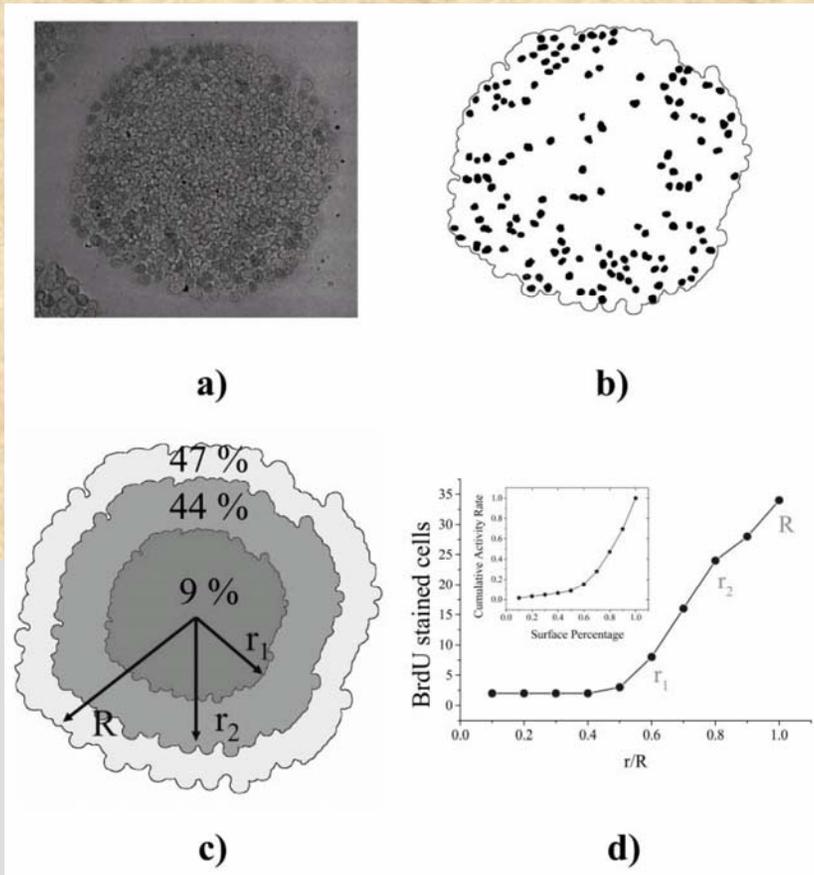
In vivo:
Filopodial
extensions
of a
sprouting tip

Green:
Endothelial
Cells (ECs)

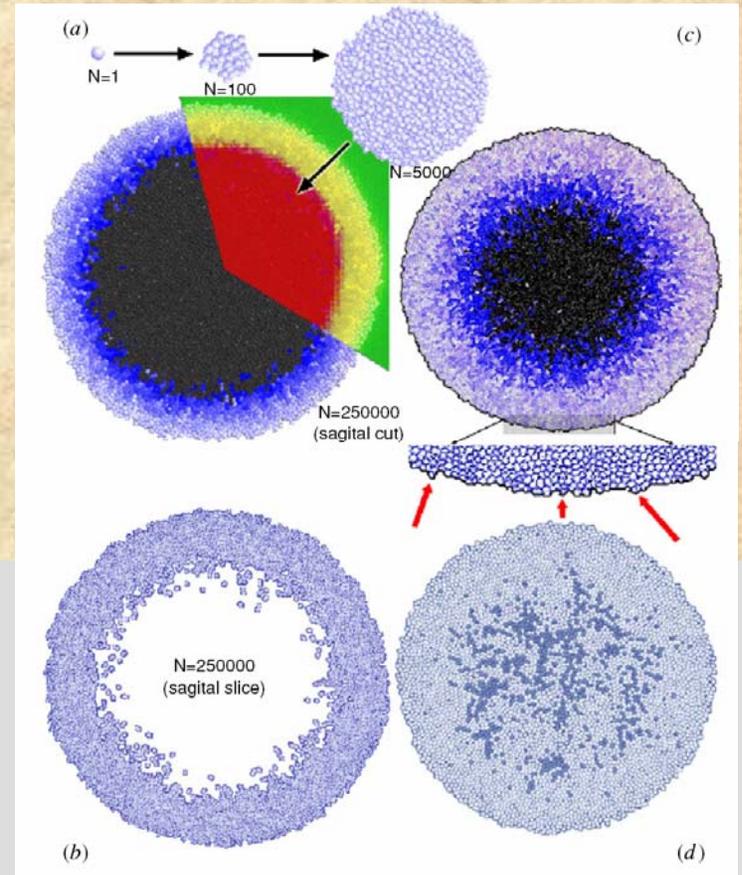
Blue:
Nuclei



Tumor cell proliferation confined to outer rim:



Experiment, Brú et al.
Biophys. J. 85, 2948 (2003)

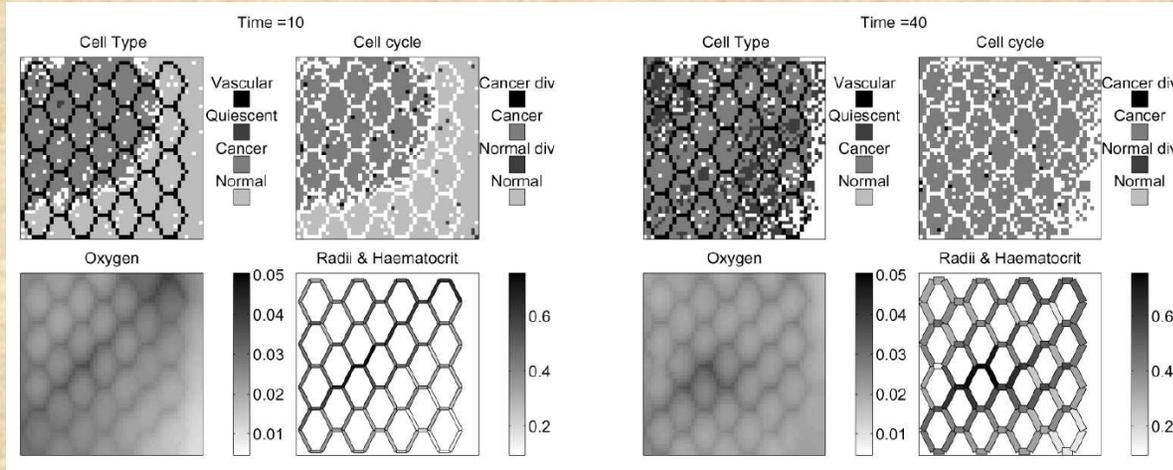


Theoretical model, Drasdo & Höhme
Phys. Biol. 2, 133 (2005)

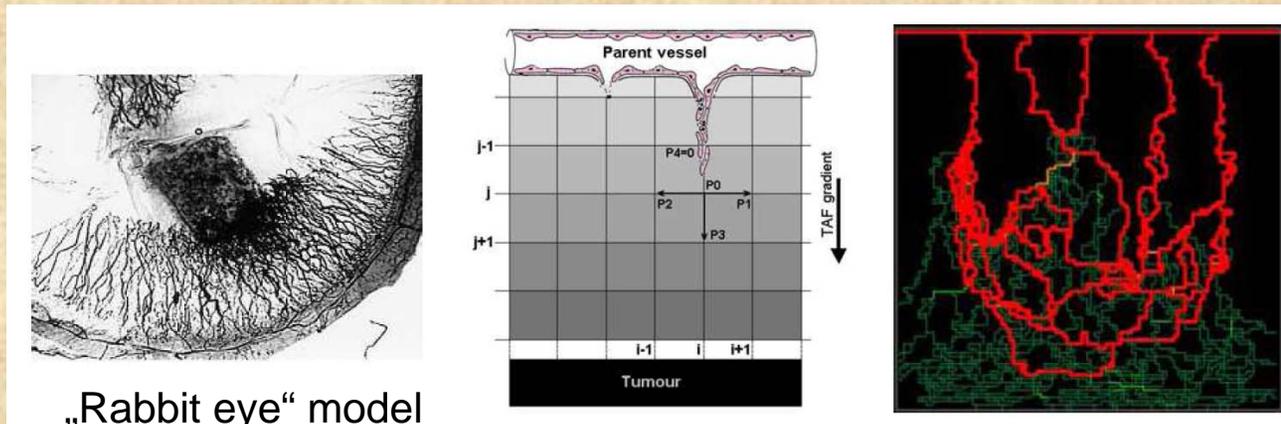
Radius of an avascular tumor in vitro grows linearly in time

Earlier theoretical work

Fixed vessel network, proliferating tumor cells (Alarcon, Byrne, Maini)



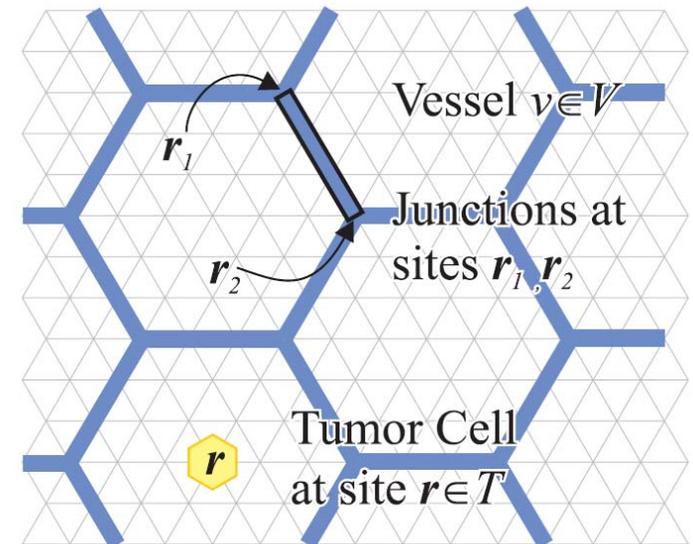
Fixed growth factor source, growing vessel network (Chaplain, Anderson, Sleeman, etc.)



„Rabbit eye“ model

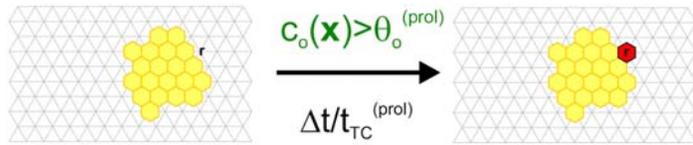
Model concept

- Network of „vessels“ = pipe and pipe-segments
- Dynamics of segments / vessels
- „Blood“ flow = ideal pipe flow
- „Tumor cells“ = cellular automaton
- Dynamics: Proliferation & death
- Vessels and tumor interact via diffusive messengers:
- Perfused vessels emit oxygen / nutrients
- Tumor cells emit growth factors

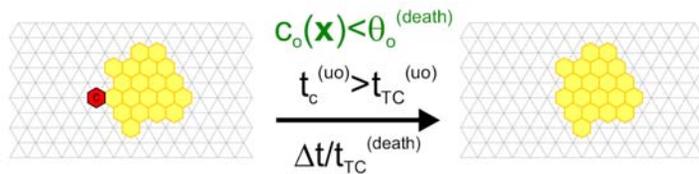


Dynamic processes (stochastic):

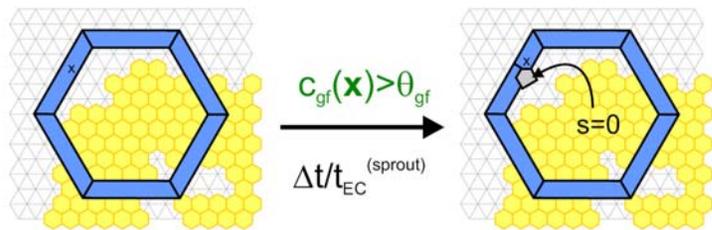
(a) TC Proliferation if sufficient O_2



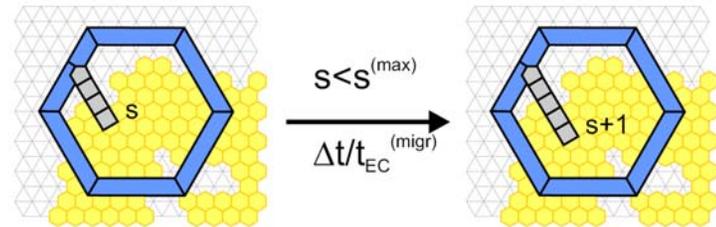
(b) TC Death if hypoxic for longer than $t_{TC}^{(uo)}$



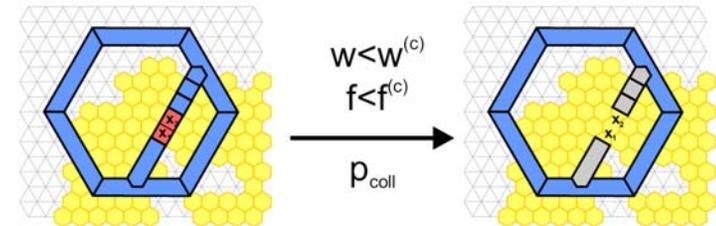
(c) Sprouting: Append segment if sufficient GF and r not too far inside the tumor



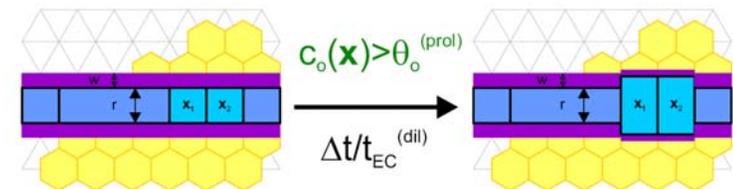
(d) Sprout extension up to max length $s^{(max)}$



(e) Regression and Collapse: Remove degenerate weakly perfused vessels



(f) Vessel dilation by Δr up to r_{max} and degeneration with rate Δw , if c_{gf} large enough



Details

Blood flow:

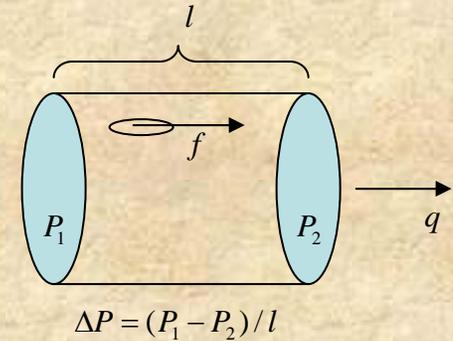
(laminar, stationary)

Effective viscosity η
from exp. Data, dep. on
radius and hematocrit

Hagen-Poiseuille

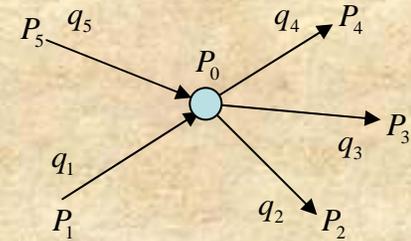
Flow rate $q(v) = (\pi/8) \frac{r^4}{\eta} \Delta P$

Shear force $f(v) = 1/2 r \Delta P$



Mass conservation

$$0 = \sum q_i = \sum const_i \cdot (P_i - P_0)$$



Oxygen / nutrient diffusion:

$$\frac{\partial c_{oxy}}{\partial t} = D \Delta c_{oxy} - c_{oxy} k(r) + J(r)$$

$$J(r) = \begin{cases} q \cdot (c_{blood} - c(r)) & \text{for } r \in v \in V \\ 0 & \text{otherwise} \end{cases}$$

$$k(r) = \begin{cases} k_0 & \text{in ECM} \\ k_1 \geq k_0 & \text{in tumor} \end{cases}$$

Growth factor diffusion:

$$\frac{\partial c_{gf}}{\partial t} = \tilde{D} \Delta c_{gf} - k_0 c_{gf} + k_1 t(r)$$

$$t(r) = \begin{cases} 1 & \text{for } r \in T \text{ and } c_{oxy}(r) < \theta_{oxy} \\ 0 & \text{otherwise} \end{cases}$$

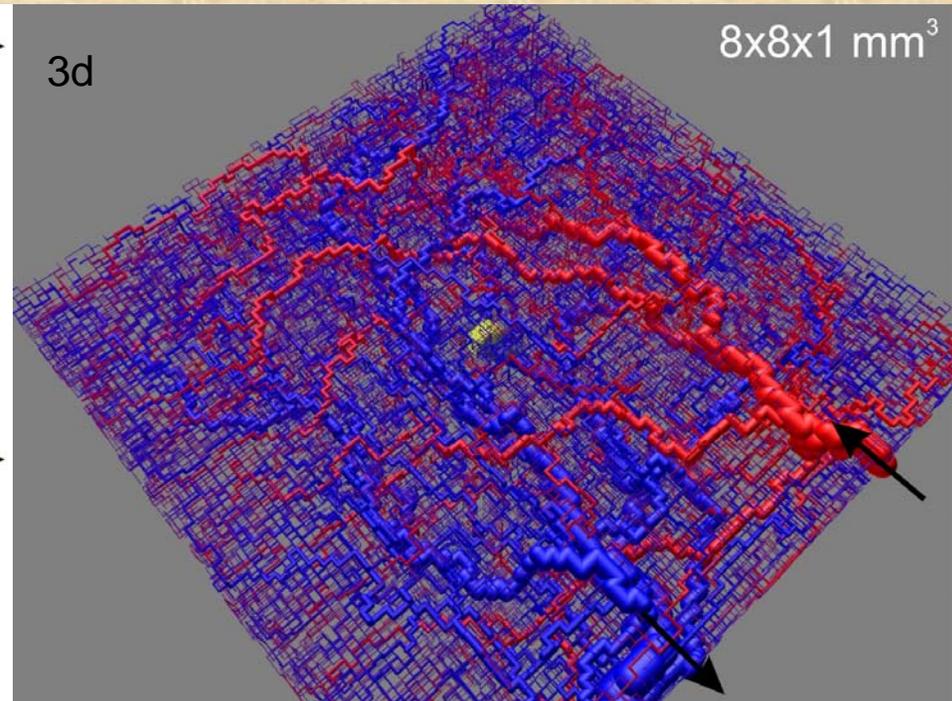
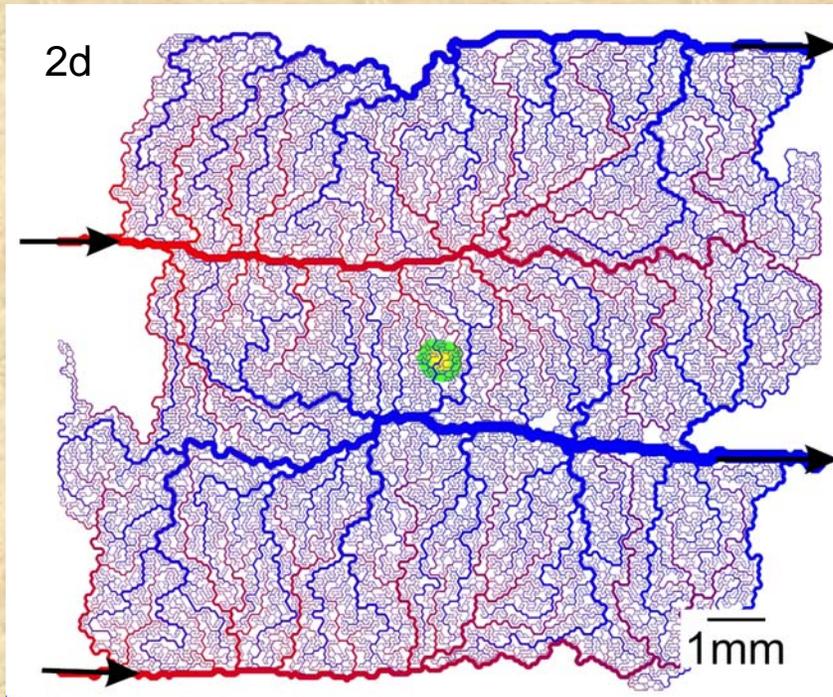
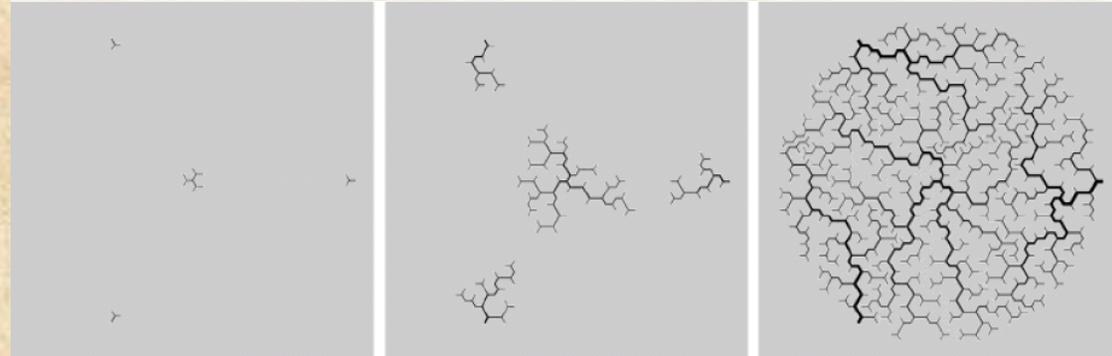
Initial arterio-venous network

2d model:

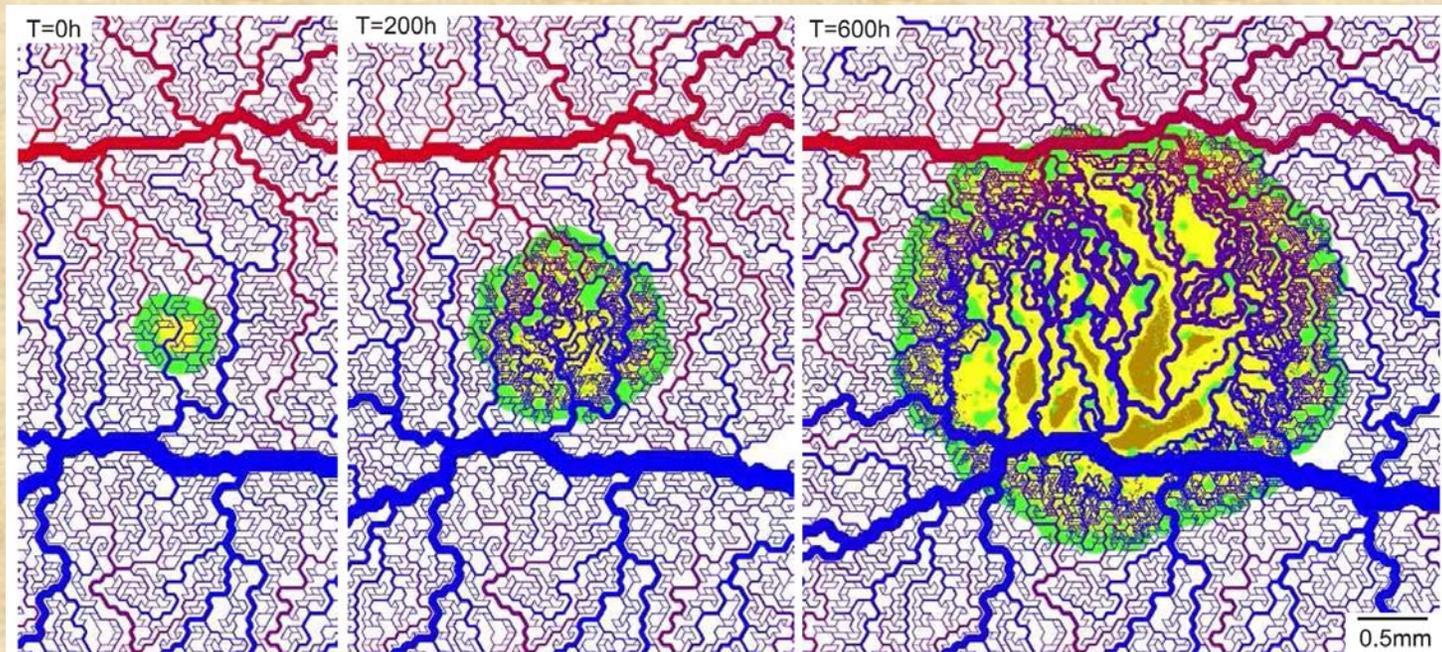
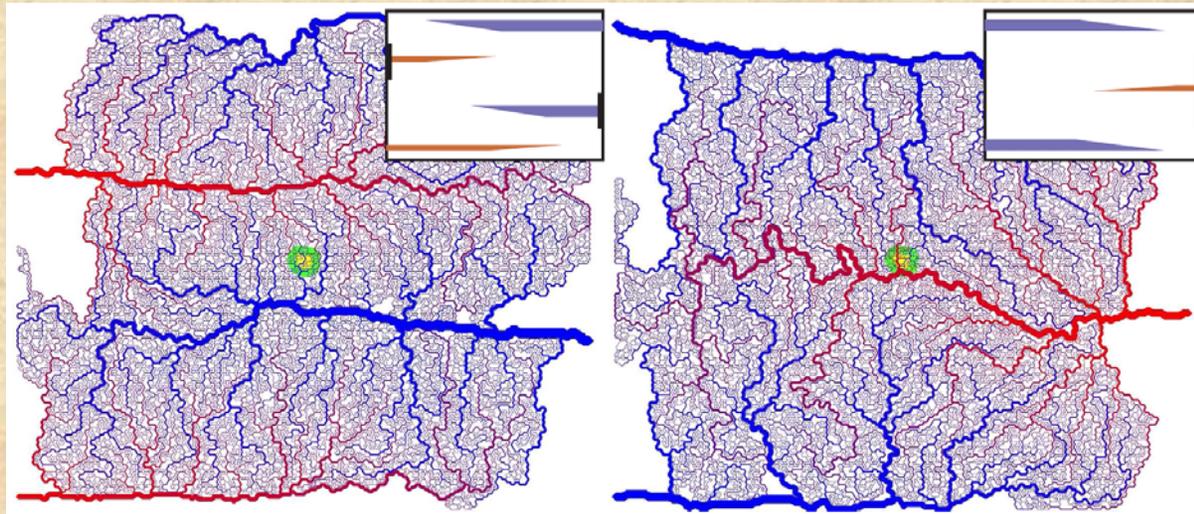
[Gödde & Kurz, Dev. Dyn 220, 387 (01)]

Branchings obey Murrays law:

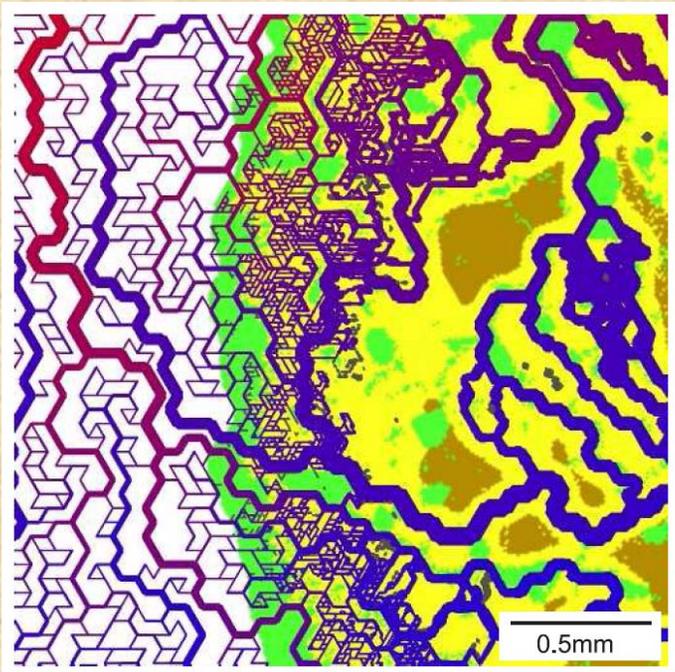
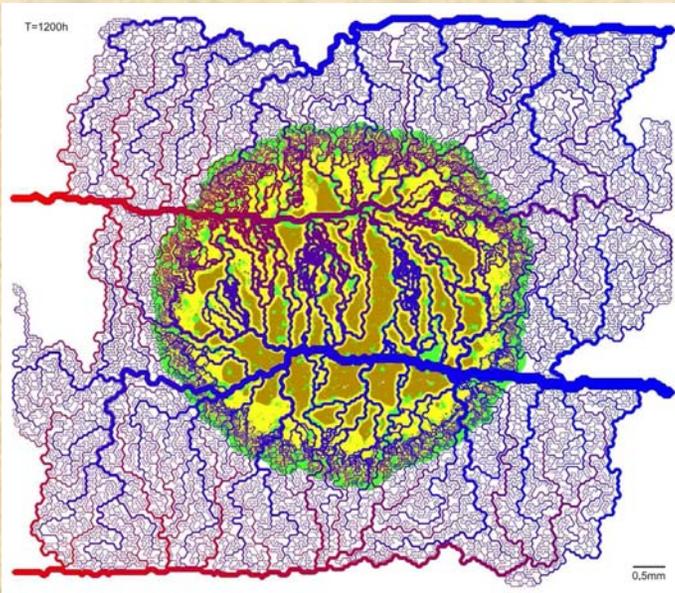
$$r_{\rho}^{\alpha} = r_1^{\alpha} + r_2^{\alpha} \quad \alpha \approx 2.7$$



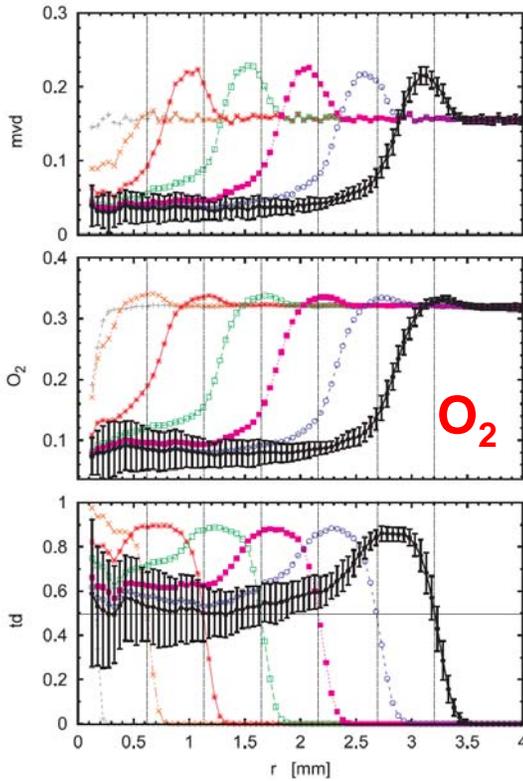
Tumor growth in arterio-venous network



Radial distributions

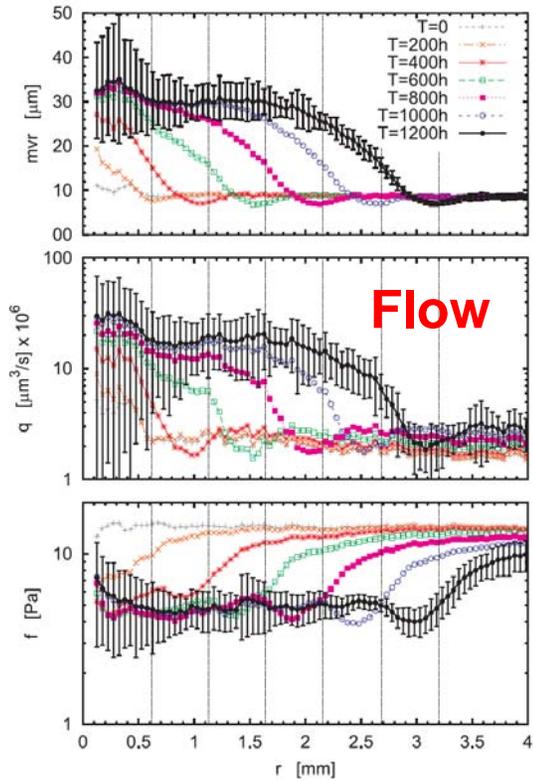


MVD



Tumor density

Vessel radius



Shear force

[Welter, Bartha, Rieger, [arXiv:0801.0654v2](https://arxiv.org/abs/0801.0654v2) [q-bio.TO]]

Comparison w. experimental data obtained on melanoma vessels

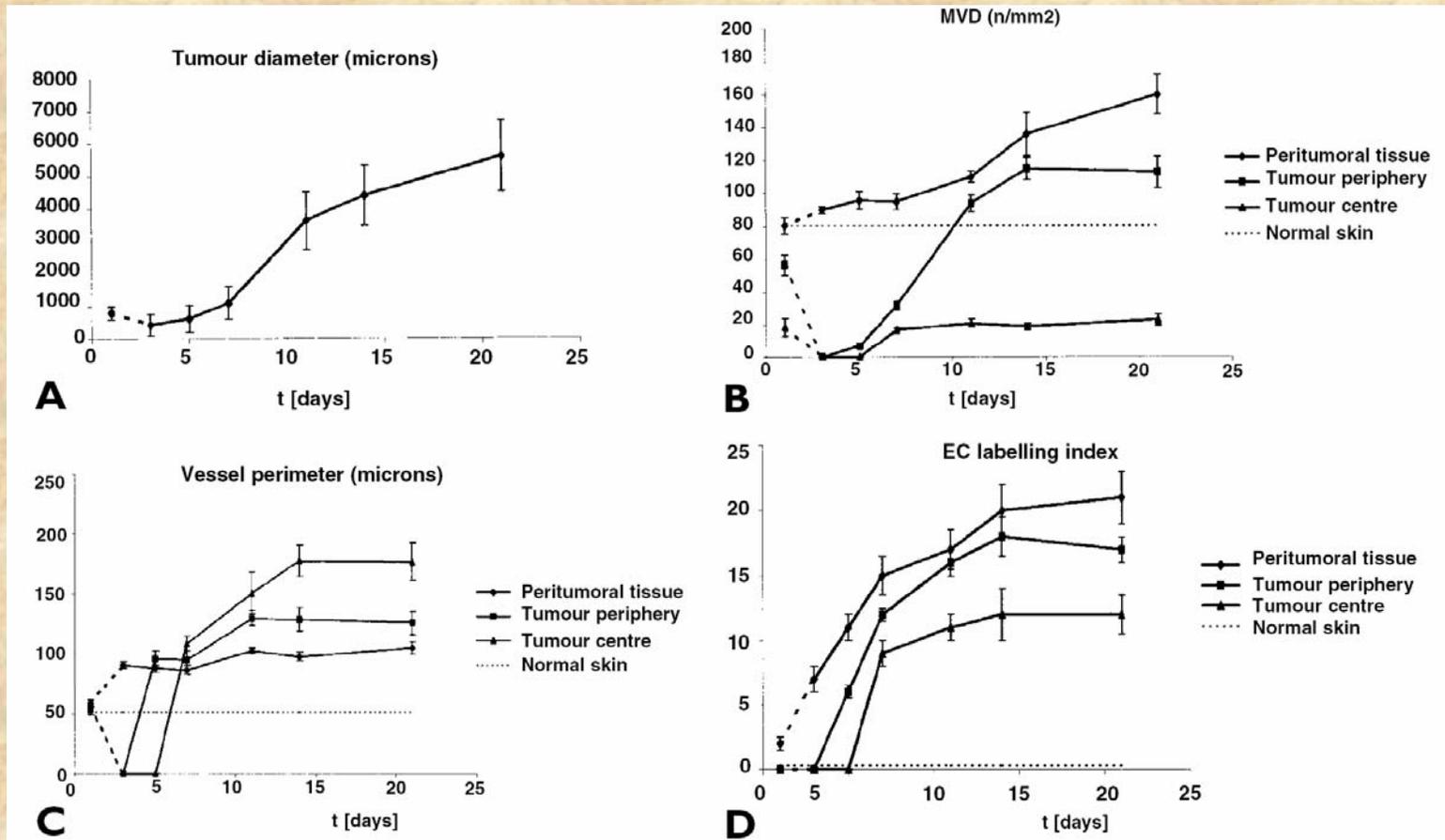
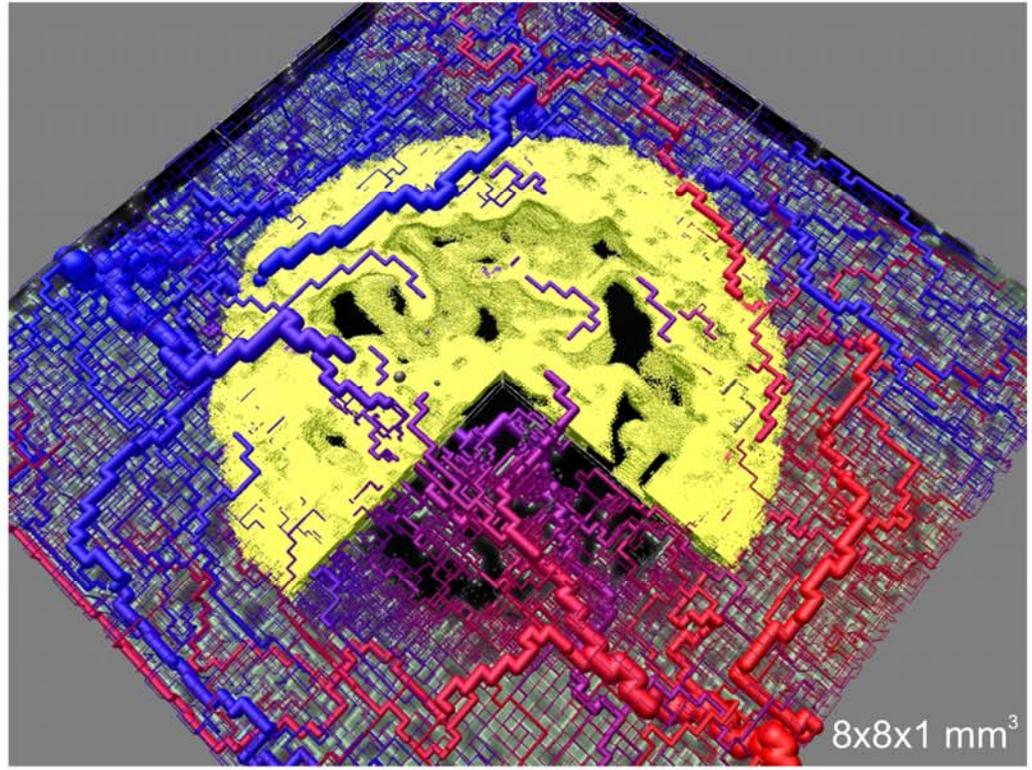
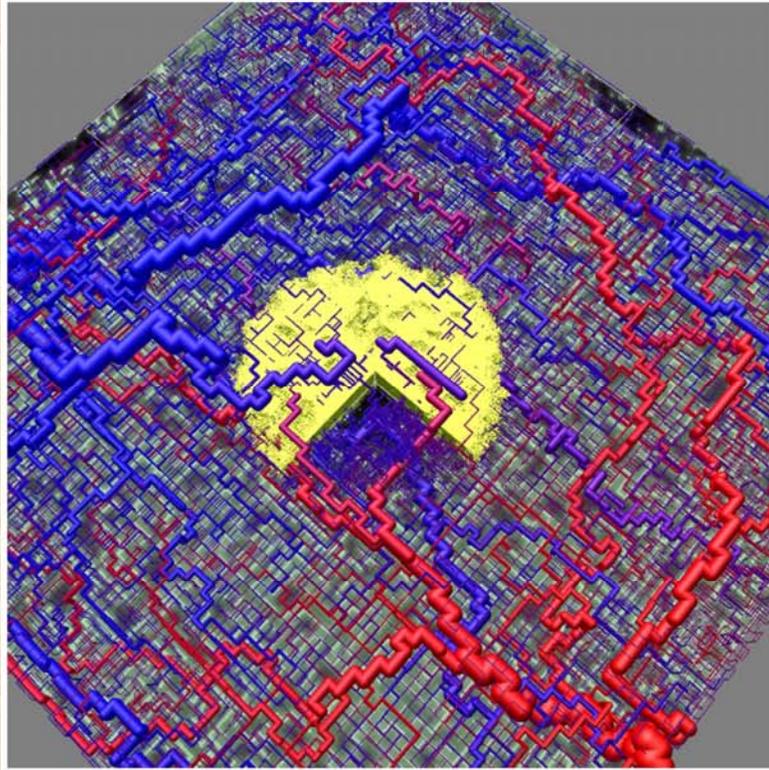
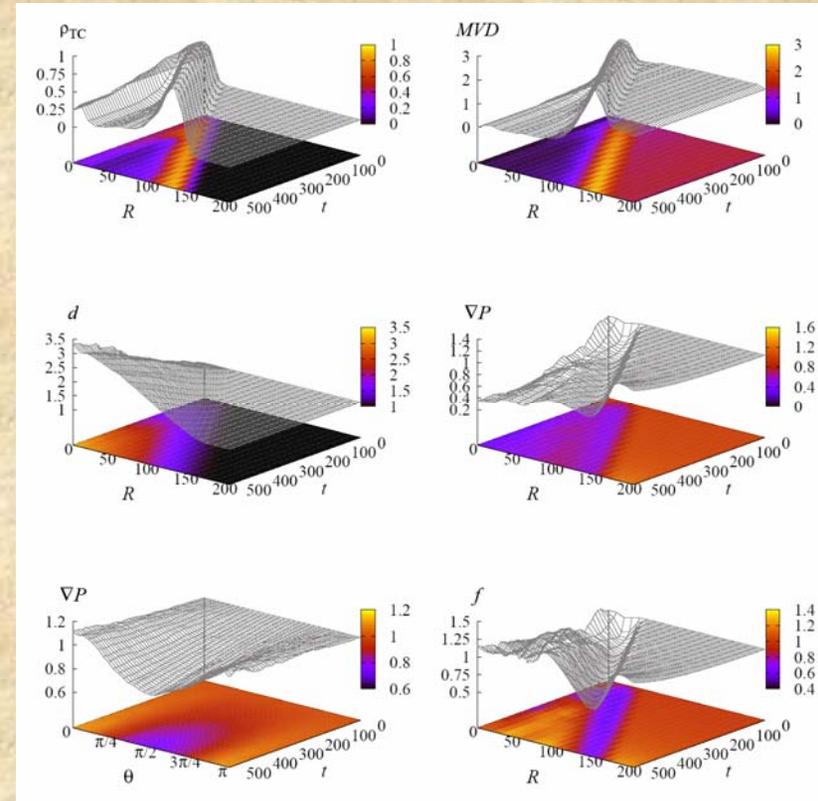
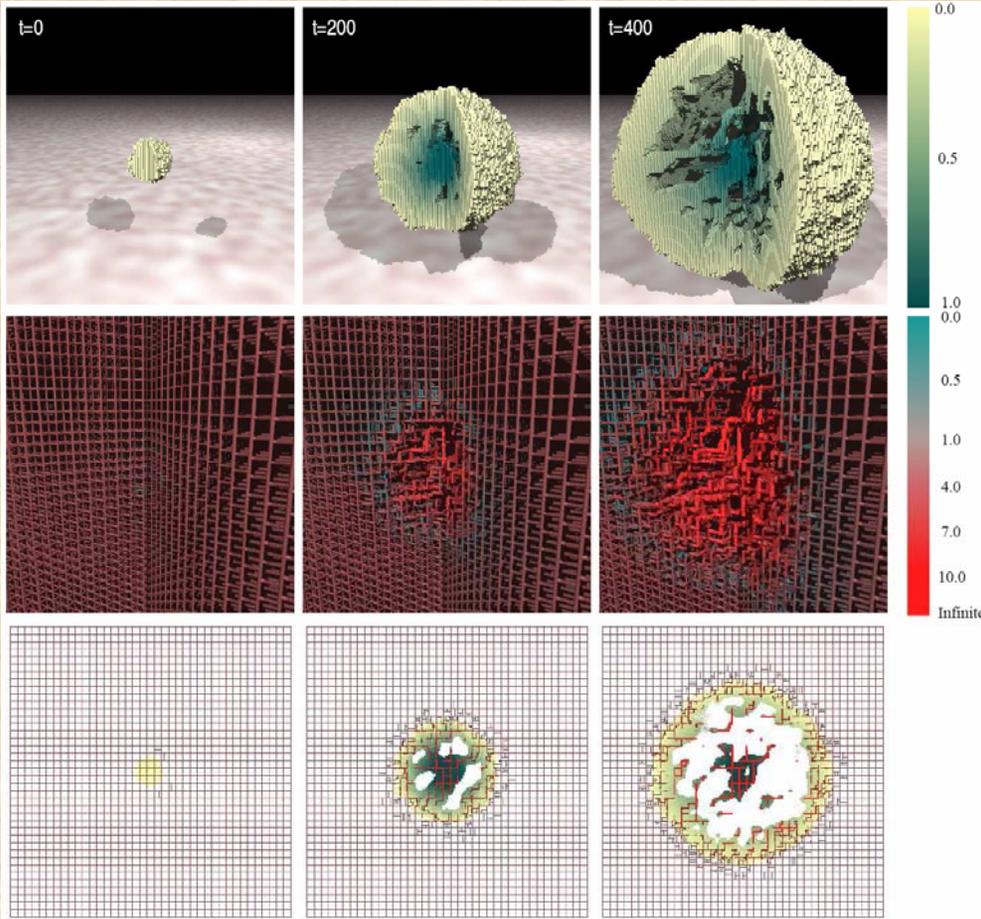


Figure 2. Tumour diameters (A) and alterations of vascular parameters (B, C, D) of B16 murine melanoma. Groups of three mice were sacrificed by anaesthesia at 1, 3, 5, 7, 11, 14 and 21 days. Data are means \pm SEM. The decrease of MVD and vessel perimeter between days 1 and 3 can be explained by the regression of the existing host vessels of the dermis, following the injection of the tumour cell suspension. The mean MVD, vessel perimeter and EC labelling index in normal mouse skin were 80.7 ± 7 , 51.5 ± 2.5 and 0.33 ± 0.15 , respectively (mean \pm SD, $n = 3$).

... in 3d (prel.)

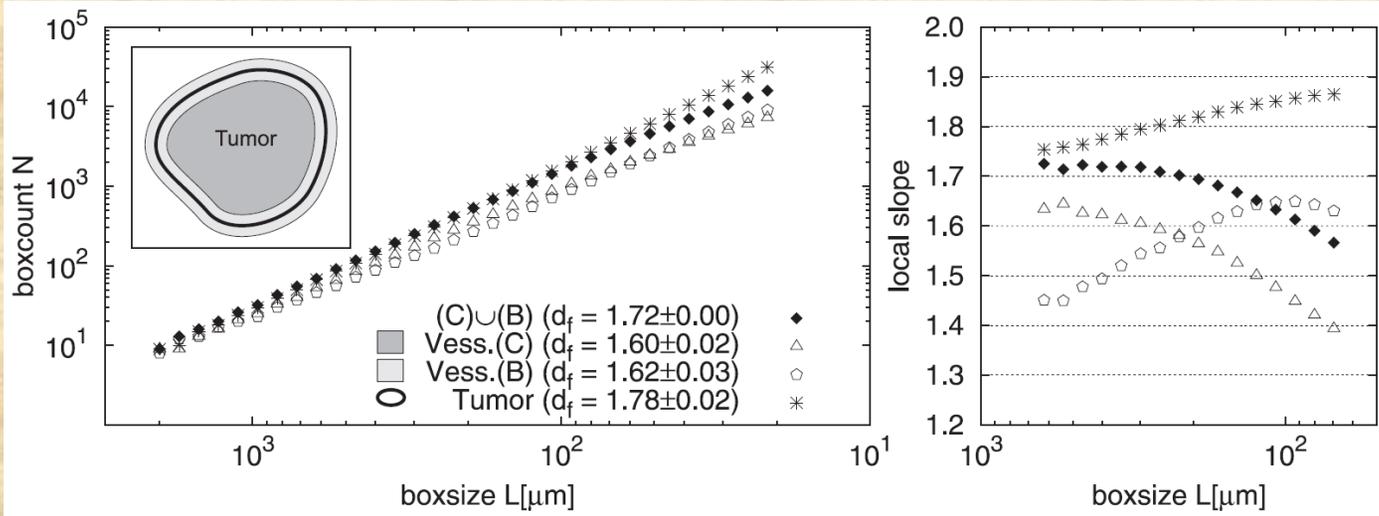


Three dimensional model for tumor vascularization:

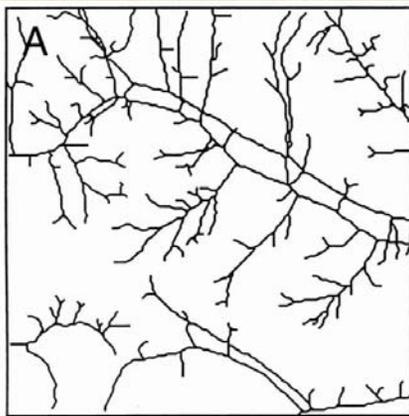


Quantitatively similar to 2d version!

Fractal analysis:



Fractal dimension
in different regions
of the tumor
Vasculature
 $D_f \sim 1.8$

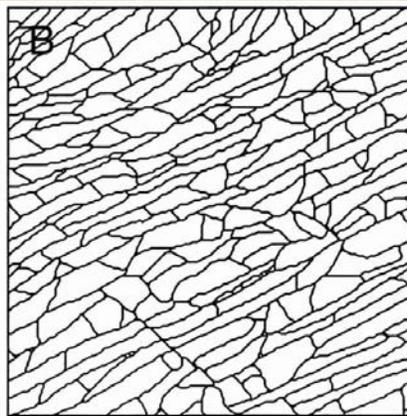


$500\mu\text{m}$

(a)

arteriovenous net.:

$d_f = 1.70 \pm 0.03$

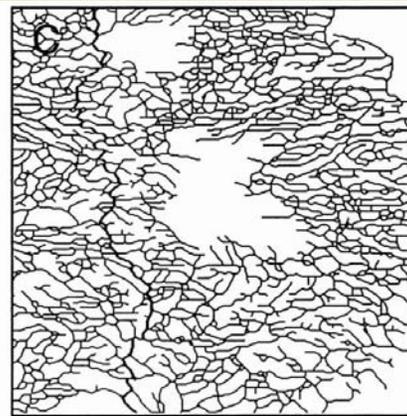


$500\mu\text{m}$

(b)

Norm. capillary net.:

$d_f = 1.98 \pm 0.02$



$500\mu\text{m}$

(c)

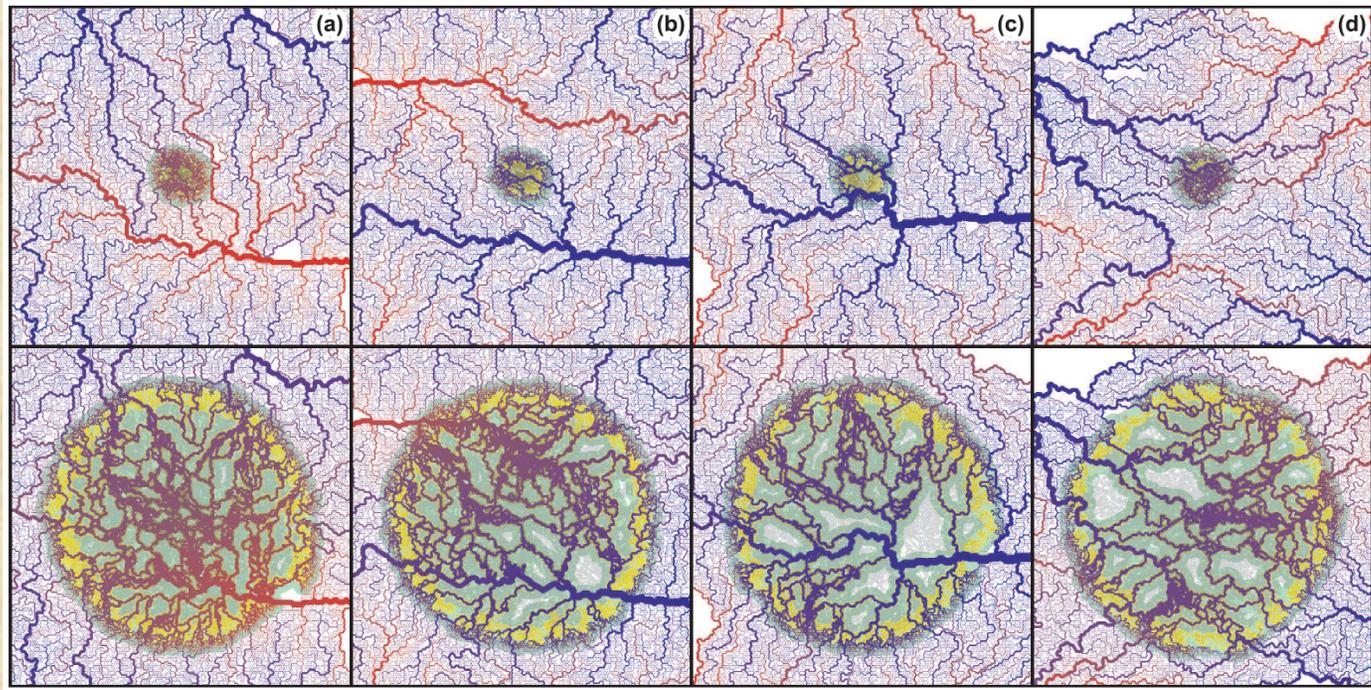
carcinoma network:

$d_f = 1.88 \pm 0.04$

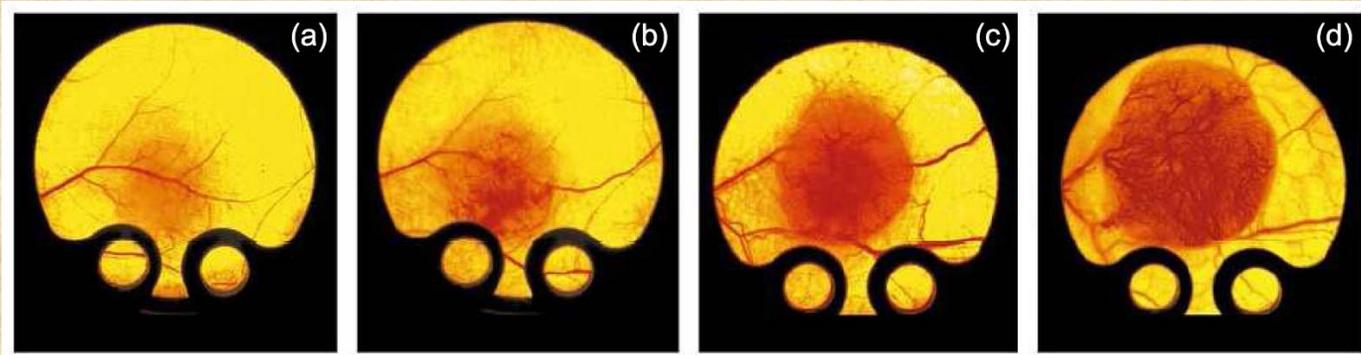
Experiment

Gazit et al.,
Phys. Rev. Lett. 75, 2428 (1995)

Formation of „hot spots“ – dependence on initial network



comparison w. experiment (dorsal skinfold chamber):

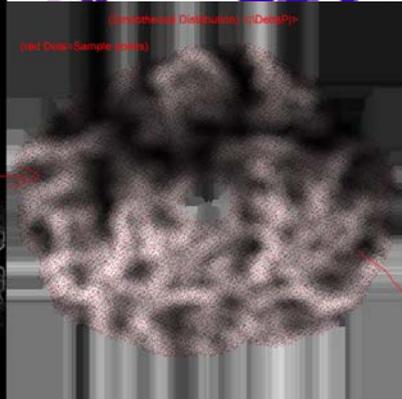
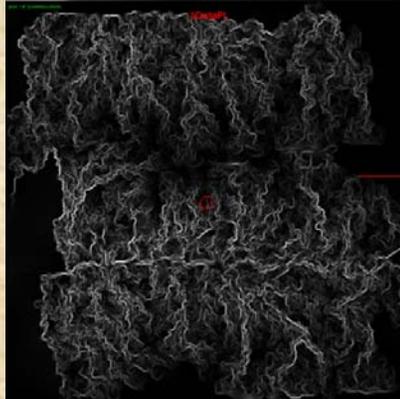
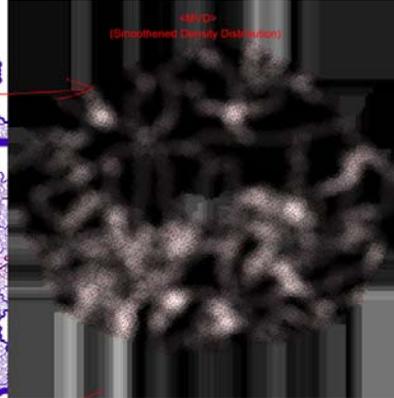
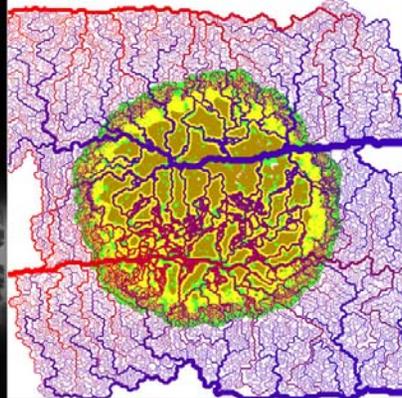
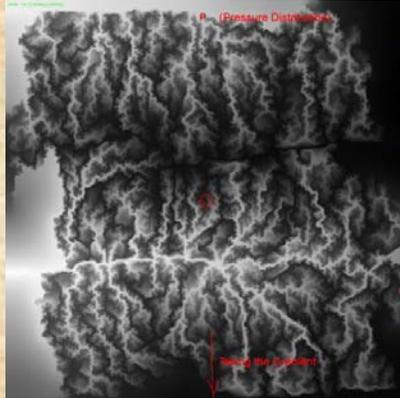


Correlation of hot-spot formation with pressure gradients

pressure in initial netw.

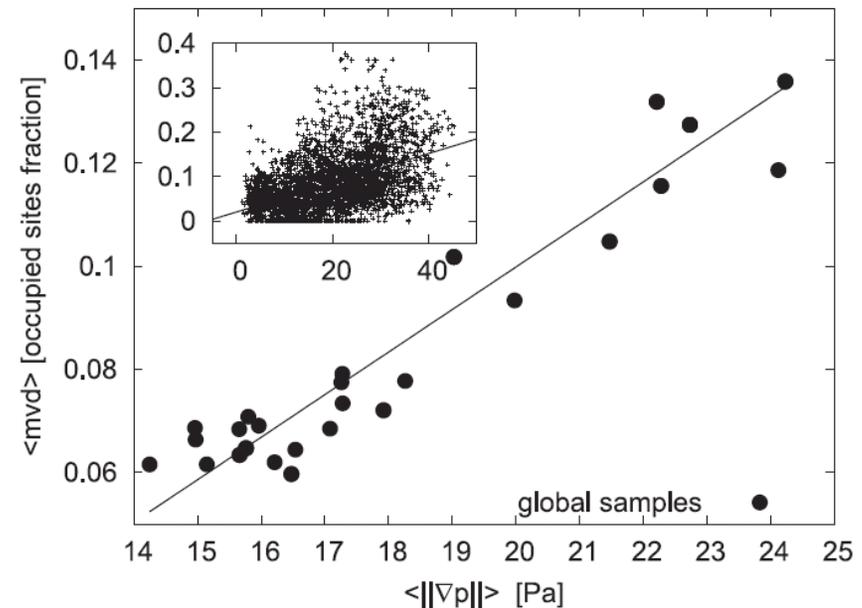
tumor network

local MVD of tumor network



pressure gradients
in initial network

pressure gradients
goarse grained

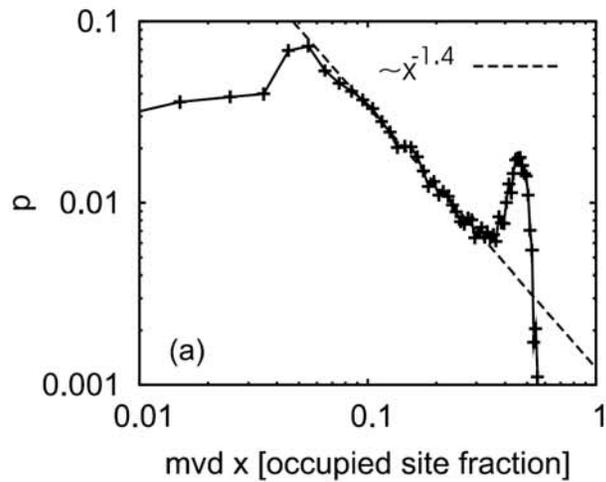


Correlation plot: local MVD in tumor network vs. local pressure gradient in initial network

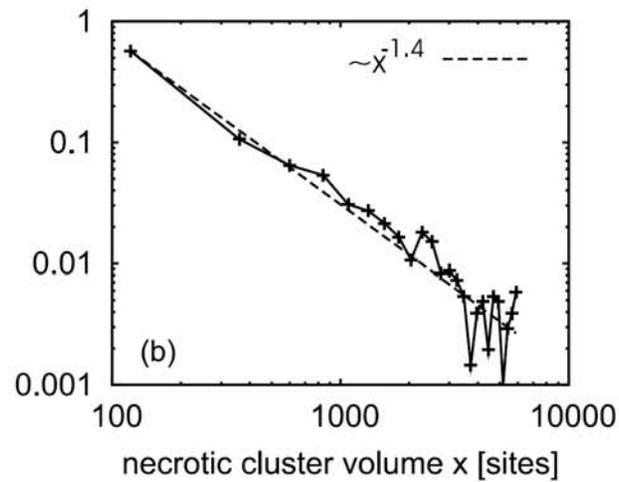
Spatial inhomogeneities display self similar behavior

Algebraic tails in probability distributions of

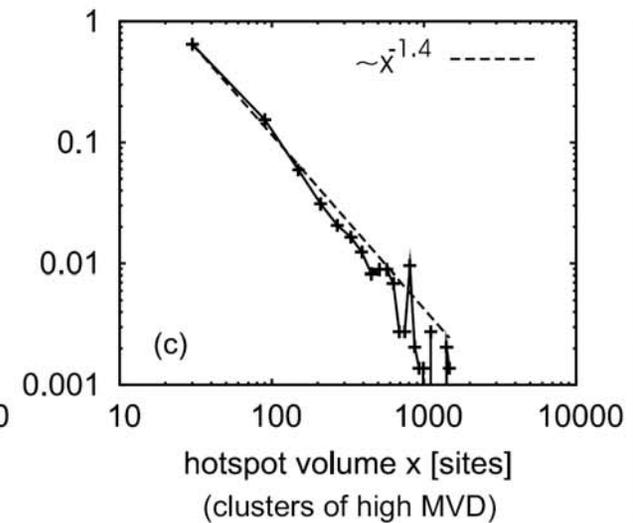
Local MVD



Size of necrotic clusters

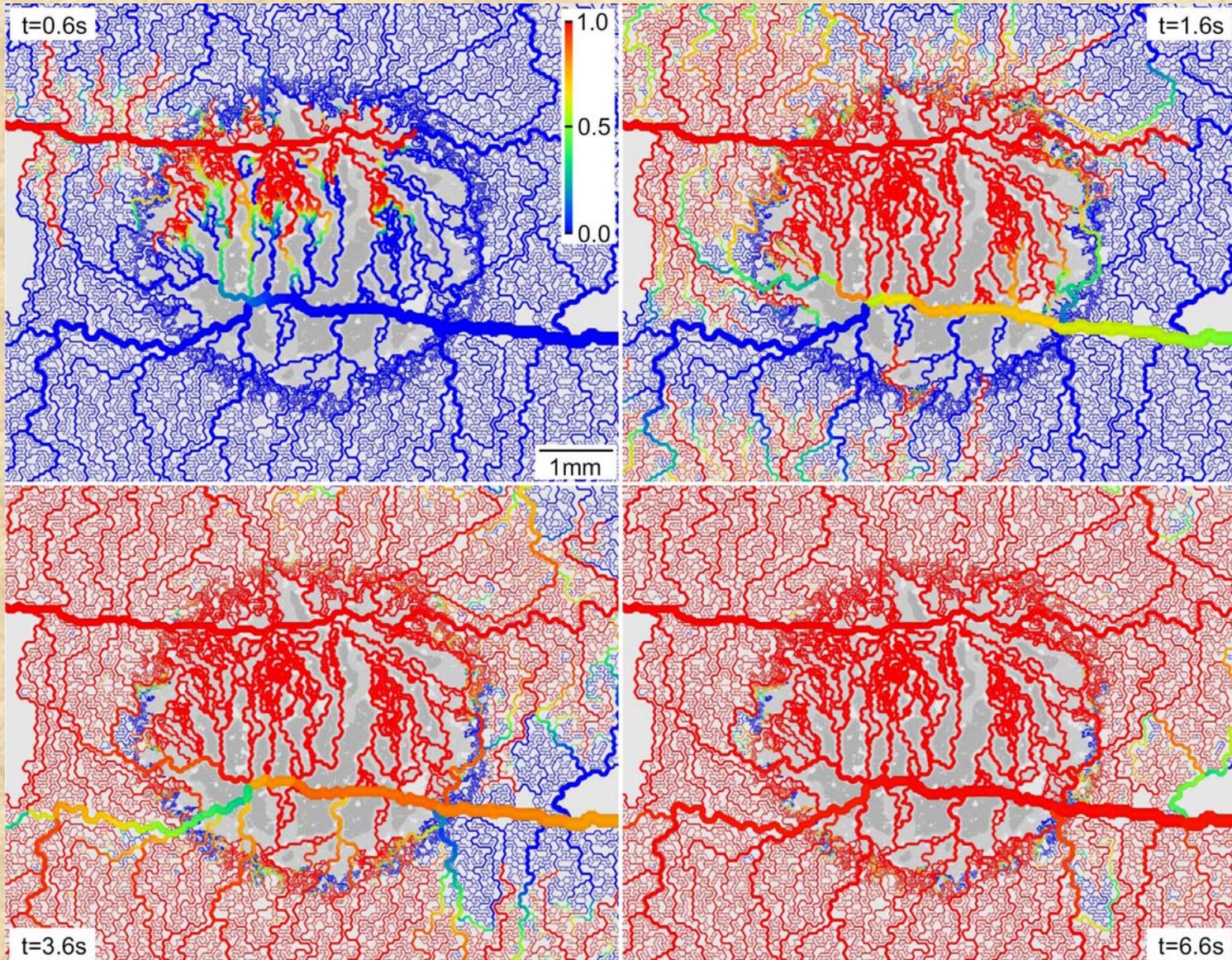


Size of hot spots

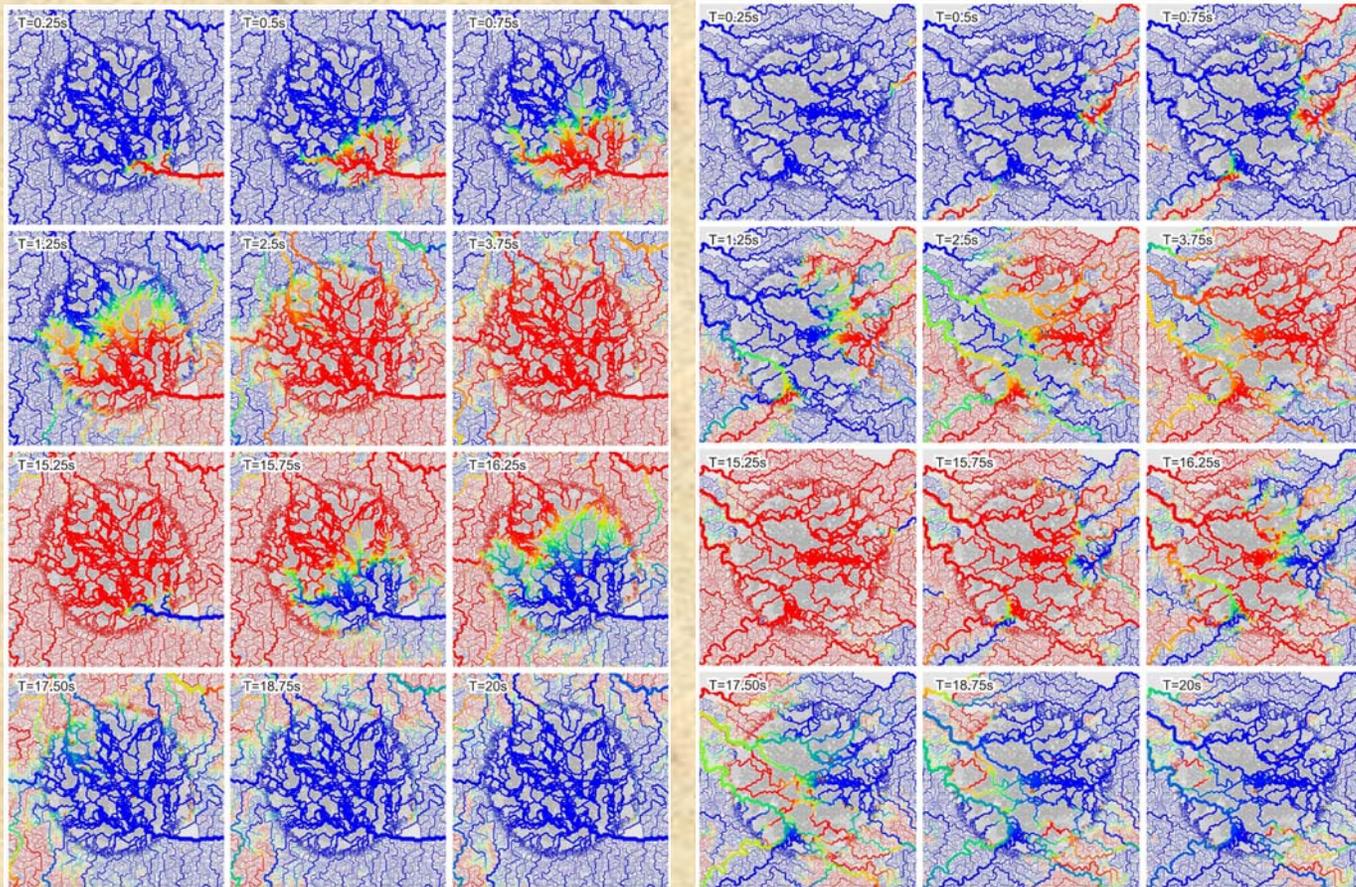


Drug flow simulation

(continuous injection into blood stream of main artery)



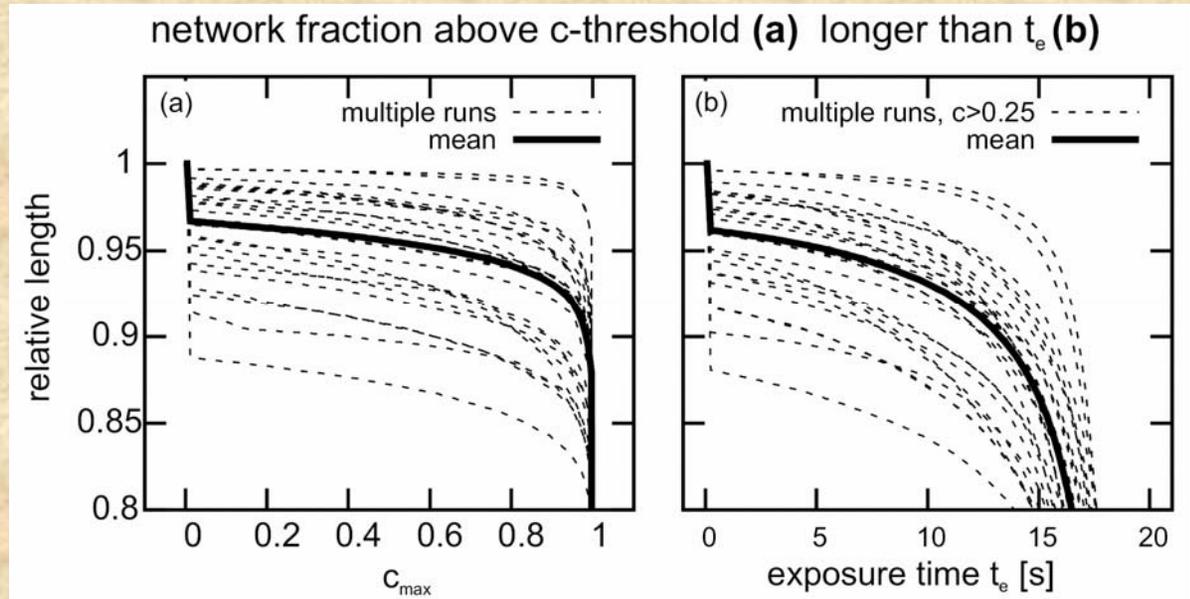
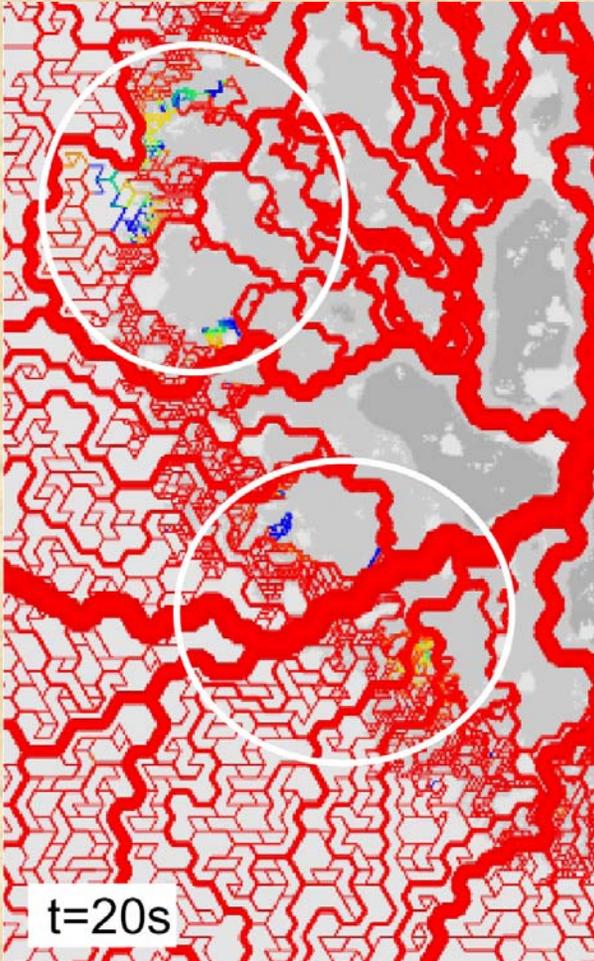
Drug flow



→ Drug reaches all vascularized regions of the tumor!
Reasons for drug delivery problems during therapy?

Drug flow (2)

Tiny nests of badly-perfused vessels in tumor periphery



Conclusions

- Morphology of tumor vasculature:
Compartmentalization into peritumoral plexus, tumor periphery and necrotic core
Result of flow-correlated percolation process, independent of initial network
- Fractal properties: Dependent upon parameters and location in tumor
Not a well defined concept in tumors
- Low pressure gradient and
small shear forces in tumor vessels
- Location of “hot spots“ of well perfused tumor regions
determined by initial network
- Drug transport through surviving tumor vessels is good
Drug delivery to TCs is known to be bad: Why?
- Next steps:
Interstitial fluid in porous medium → convective transport of drugs;
solid pressure in tumor tissue → origin of vessel collapse;
...