

# Understanding colloidal particle dynamics in microfluidic obstacle arrays with symbolic dynamics

Arnaldo Rodriguez-Gonzalez<sup>†</sup>

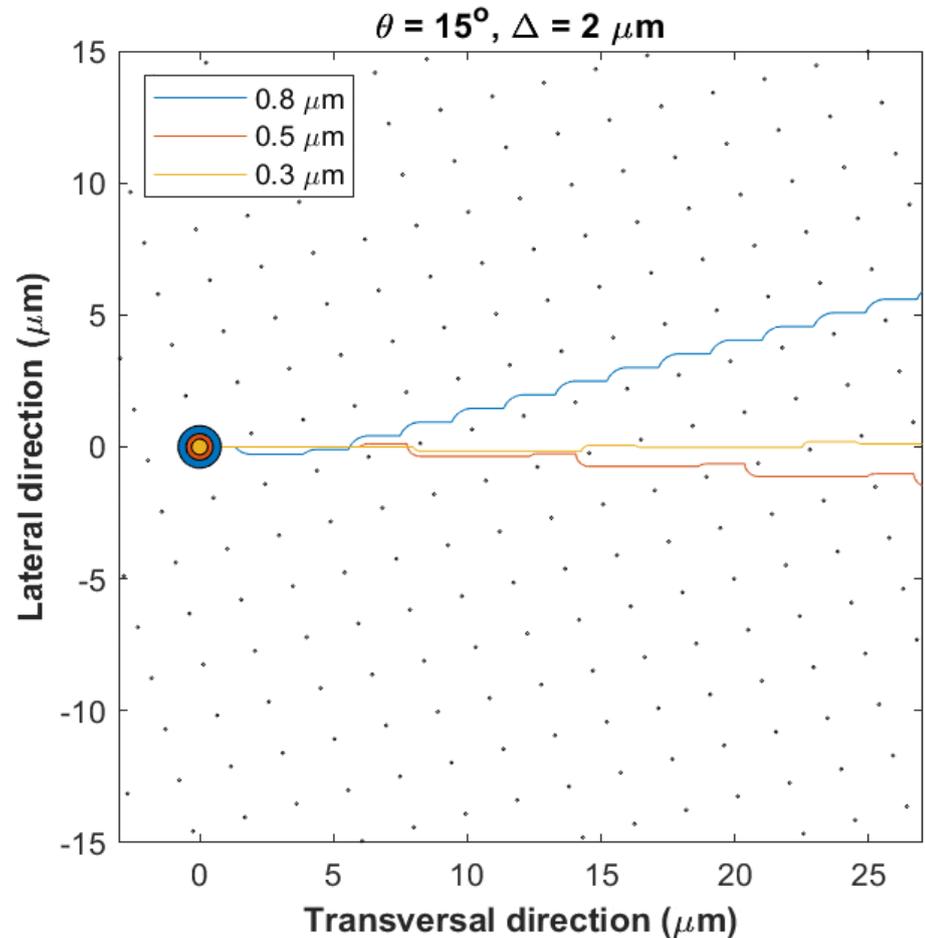
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# Prelude: laminar flow of colloidal particles through a long pipe should be straightforward



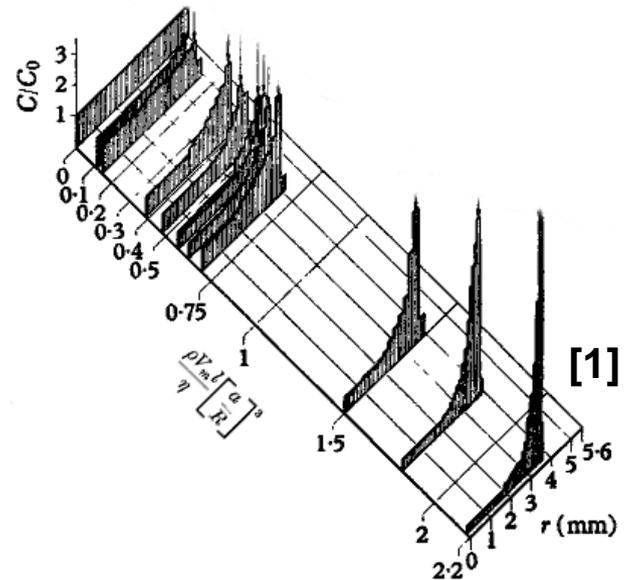
**Laminar & fully developed flow → no nonlinearities in the Navier-Stokes equations.**

$$\mu \nabla^2 \vec{u} = \nabla p$$

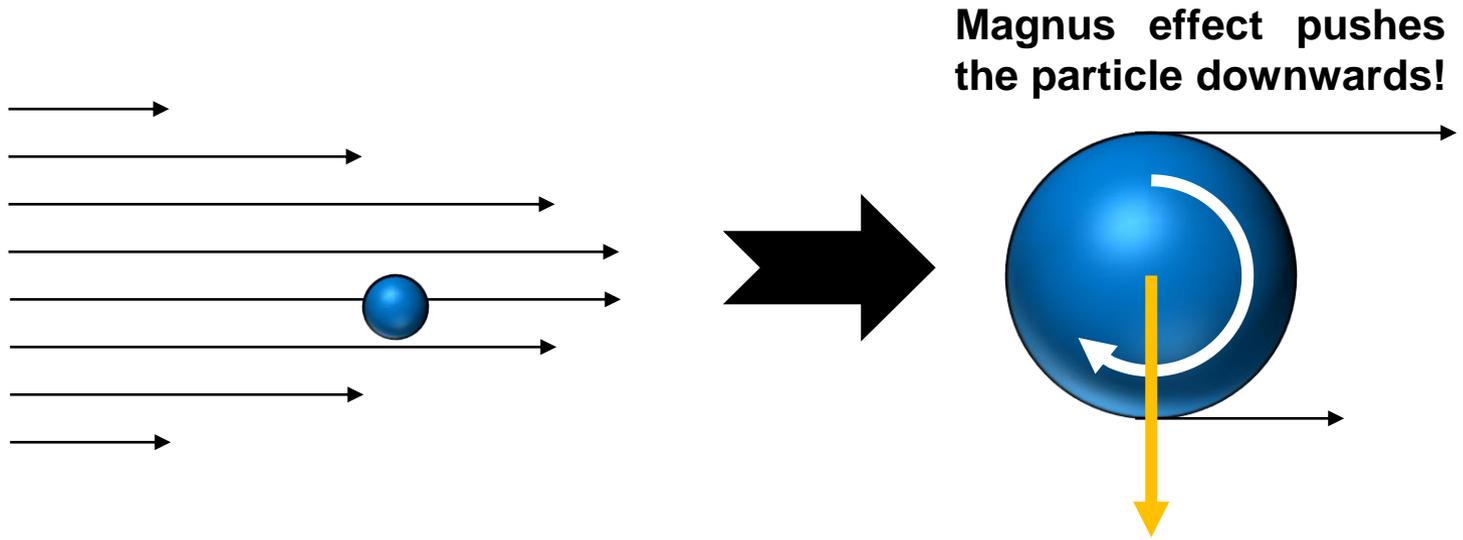
# Prelude: laminar flow of colloidal particles through a long pipe should be straightforward, but isn't



Particles laterally and *irreversibly* flow into a specific annular region within the pipe (Segré-Silberberg effect)!



# Inertial effects can play a significant role even in low Reynolds number systems



**Moral of the story:  
Particle inertia + colloidal dispersion  
= macroscale inertial effects even in  
low-Re systems!**

# Colloidal particles flowing through a channel will displace laterally when interacting with an obstacle

Expectation for low Reynolds number

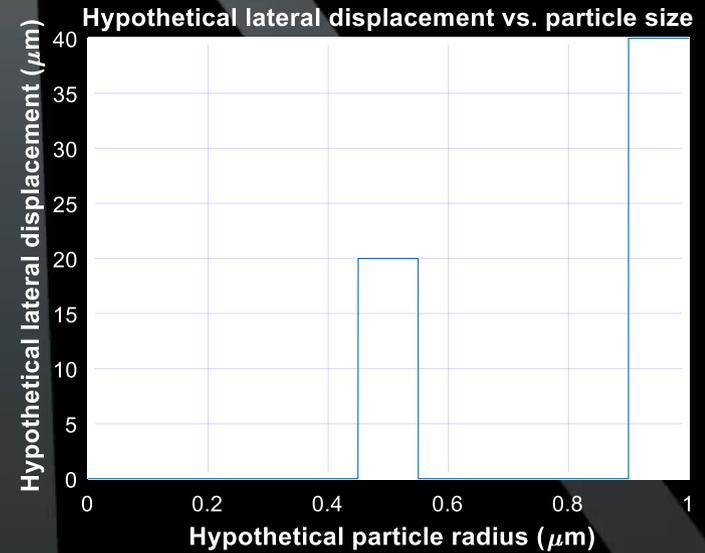


What usually happens



# Colloidal particles flowing through an obstacle-patterned channel show size-dependent dynamics

[2]



Deterministic lateral displacement<sup>[3]</sup>  
(DLD)

# The dynamics of a colloidal particle in a fluid are very complicated

The Maxey-Riley (or Basset-Boussinesq-Oseen) equation<sup>[4]</sup>:

$$\begin{aligned}
 & \text{Particle acceleration} \quad \text{Local fluid acceleration} \quad \text{Added-mass effect (accounts for fluid mass displaced by particle)} \\
 & \downarrow \quad \swarrow \quad \downarrow \\
 m_p \dot{\mathbf{v}} = & m_f \frac{D}{Dt} \mathbf{u}(\mathbf{r}(t), t) - \frac{1}{2} m_f \left( \dot{\mathbf{v}} - \frac{D}{Dt} \left[ \mathbf{u}(\mathbf{r}(t), t) + \frac{1}{10} a^2 \nabla^2 \mathbf{u}(\mathbf{r}(t), t) \right] \right) \\
 & - 6\pi a \rho_f \nu \mathbf{q}(t) + (m_p - m_f) \mathbf{g} + \boldsymbol{\delta}(\mathbf{r}(t)) - 6\pi a^2 \rho_f \nu \int_0^t d\tau \frac{d\mathbf{q}(\tau)/d\tau}{\sqrt{\pi\nu(t-\tau)}} \\
 & \nearrow \quad \nearrow \quad \uparrow \quad \nwarrow \\
 \text{Drag (Stokesian)} \quad & \text{Buoyancy} \quad \text{Particle-obstacle contact force} \quad \text{Basset force (accounts for time-lag in boundary layer development lag)}
 \end{aligned}$$

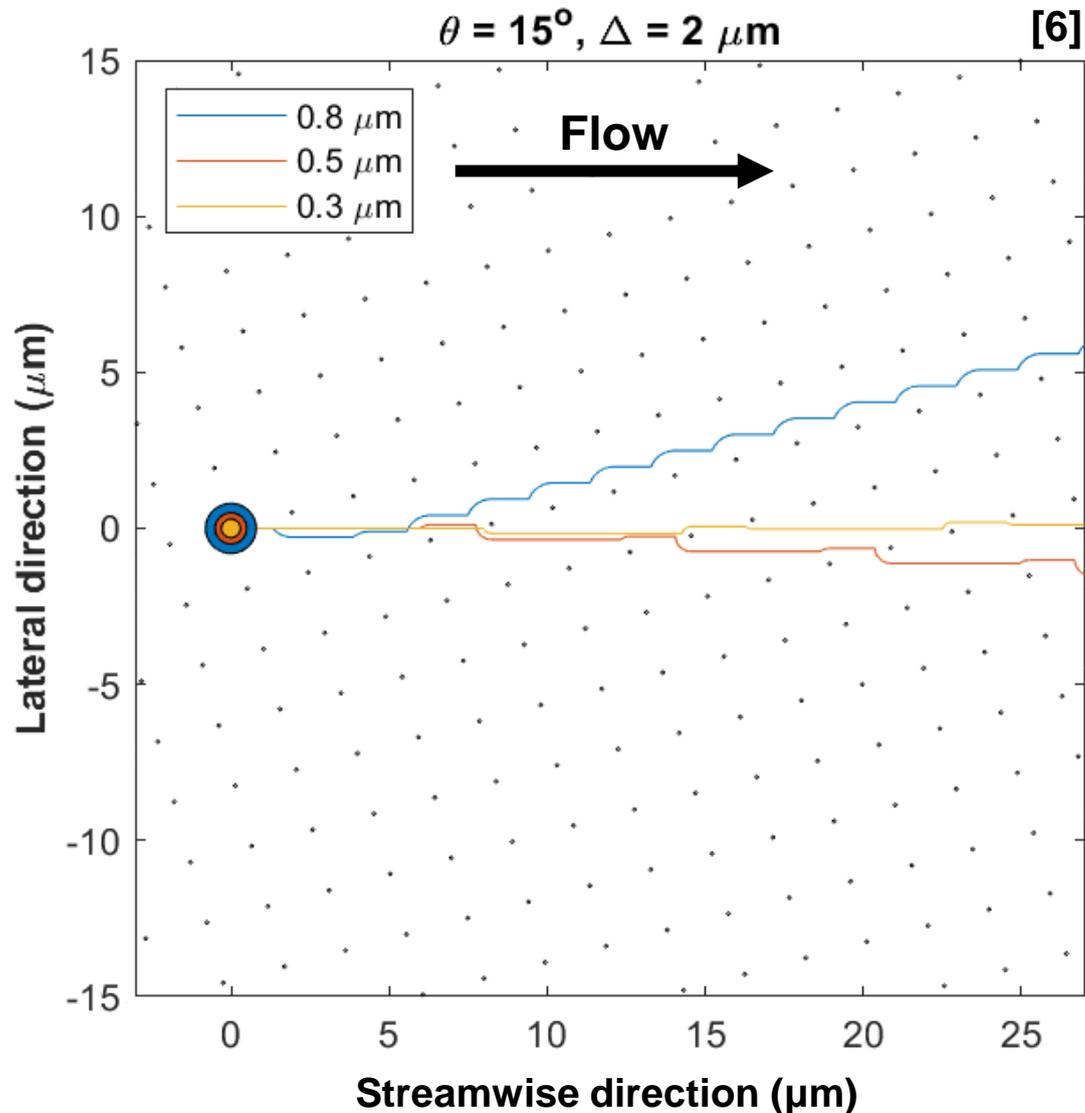
$$\mathbf{q}(t) \equiv \mathbf{v}(t) - \mathbf{u}(\mathbf{r}(t), t) - \frac{1}{6} a^2 \nabla^2 \mathbf{u}$$

# We have taken complicated analyses of particle motion through these lattices and simplified it into a dynamical sequence

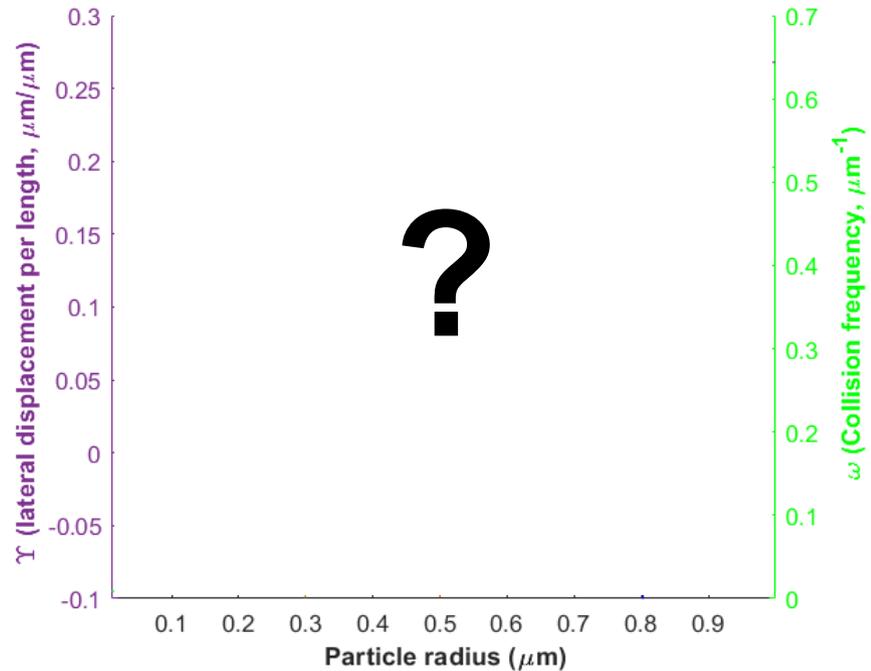
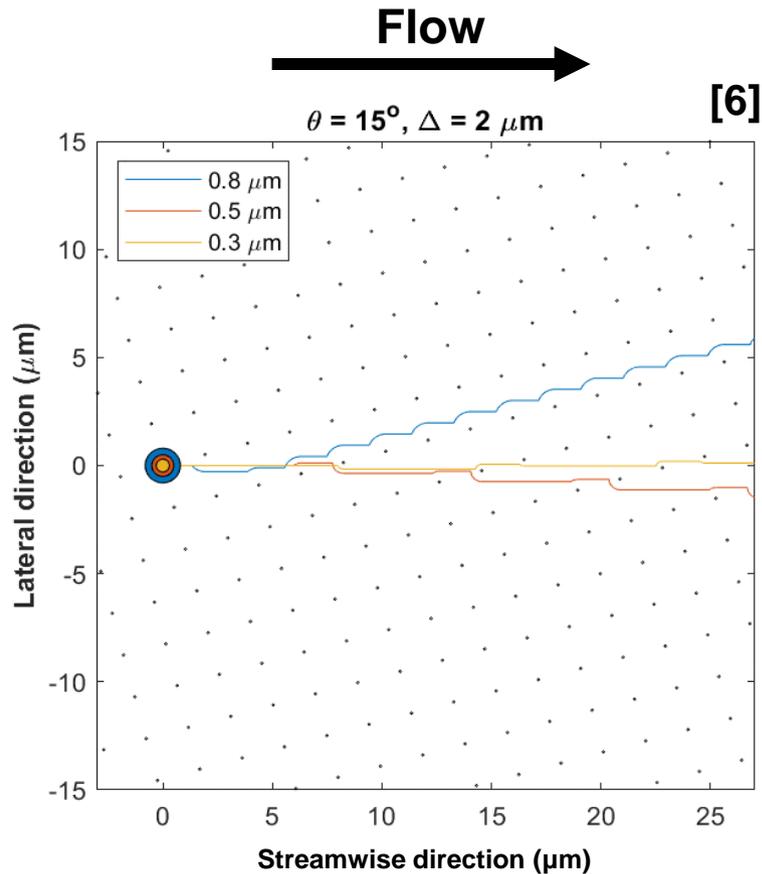
- **Assumptions we make:**
  - Peclét number is large
  - Obstacles are negligibly small
  - Particle-particle interactions are negligible
  - Particle-obstacle interactions are modeled as hard-sphere repulsion forces<sup>[5]</sup>
- **With these assumptions, trajectories can be approximated as purely streamwise advection plus a sequence of lateral displacements from collisions!**



# This simplified dynamical model reproduces deterministic lateral displacement



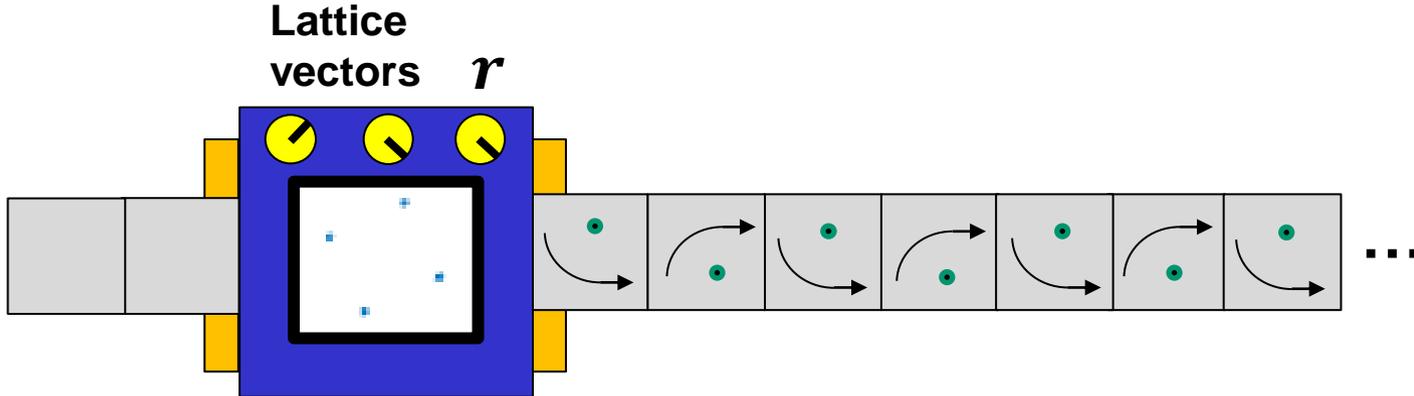
# Our goal was to construct a theory that allowed us to obtain key dynamical readouts as a function of particle size & lattice geometry



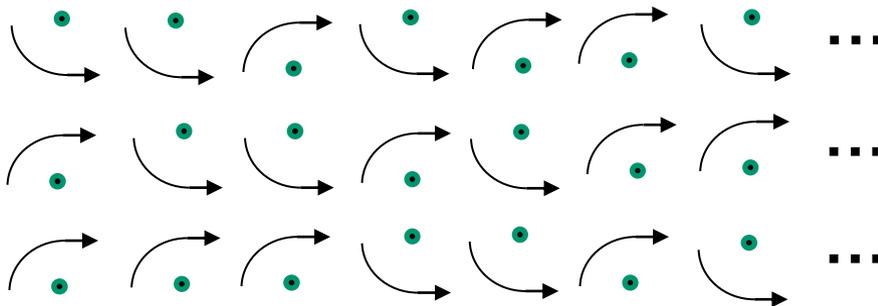
# Our model describes colloidal particle advection through lattices as a discrete sequence of collision outcomes using symbols

- After colliding with an obstacle, the particle displaces either up or down a distance of  $r$  from the obstacle it collided with.

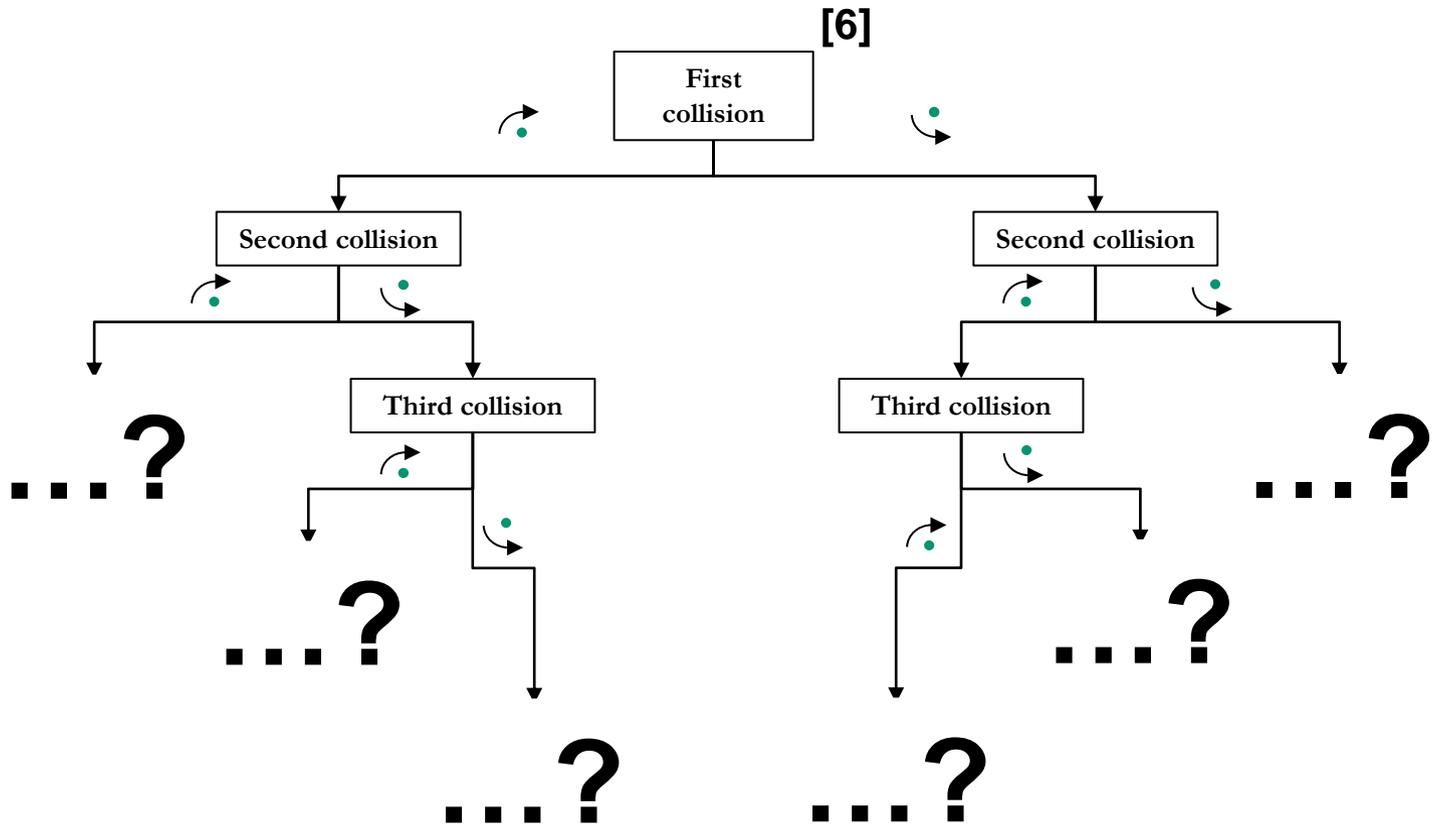
–  or 



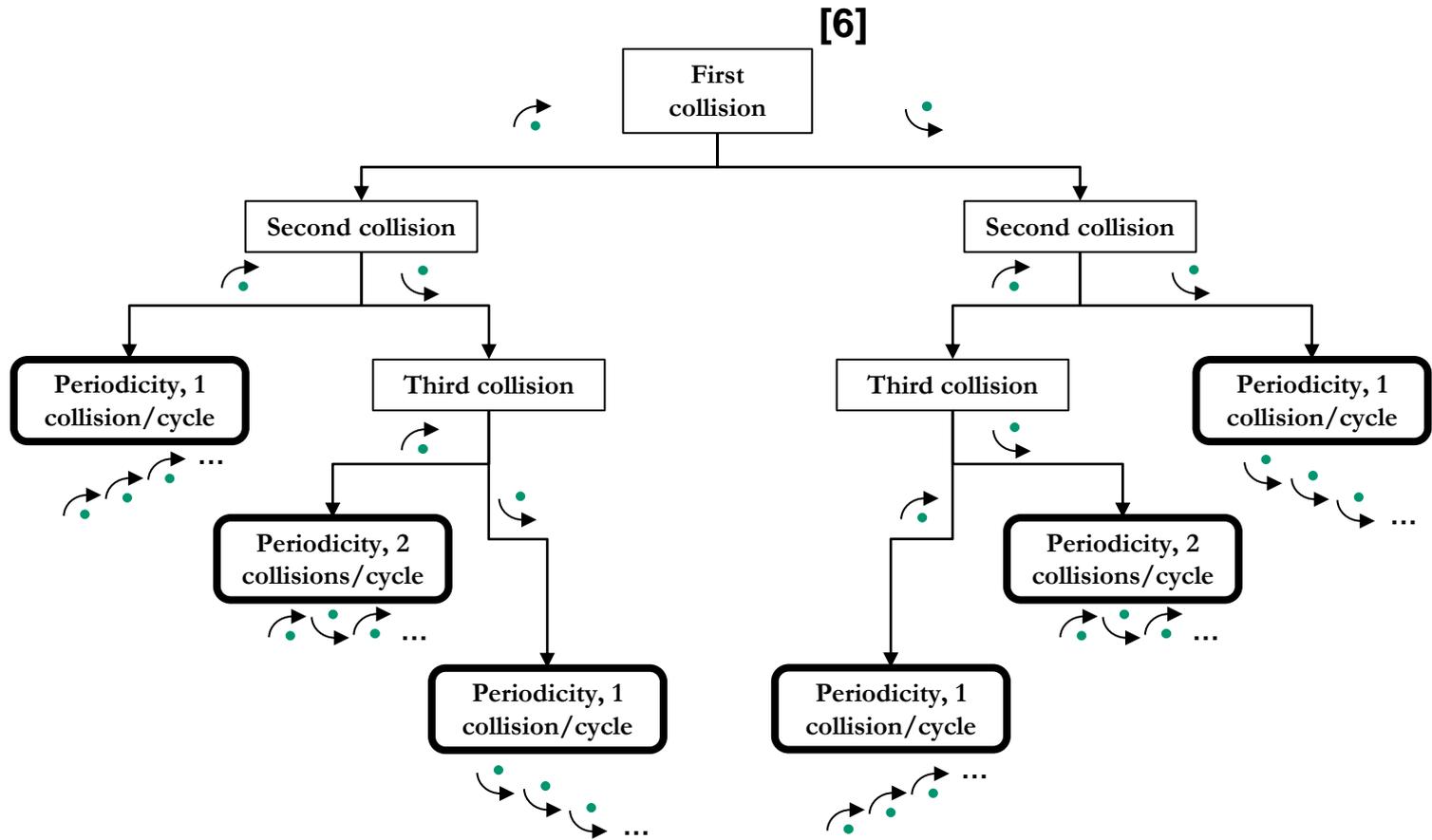
What sequences can occur?



# The spatial symmetry of the collisions heavily restricts the kinds of paths the particles can take

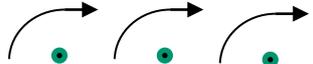


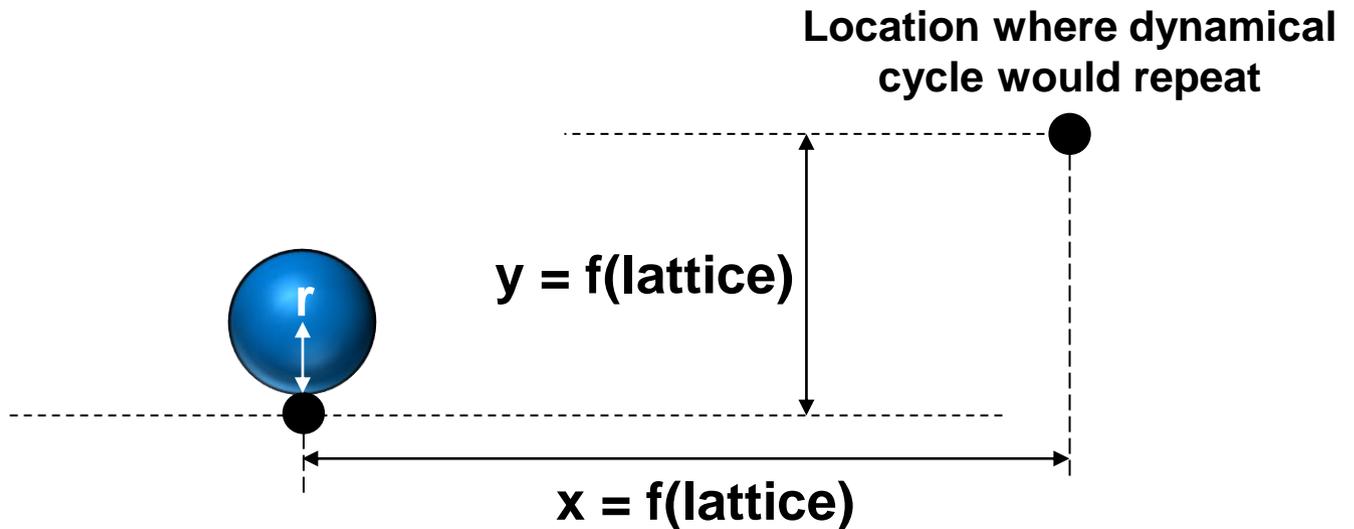
# The spatial symmetry of the collisions heavily restricts the kinds of paths the particles can take



First observed in [7], we term the general phenomenon  
“symmetry-induced cyclical dynamics”

# After determining which orbits are possible, we can determine the conditions needed for each to occur

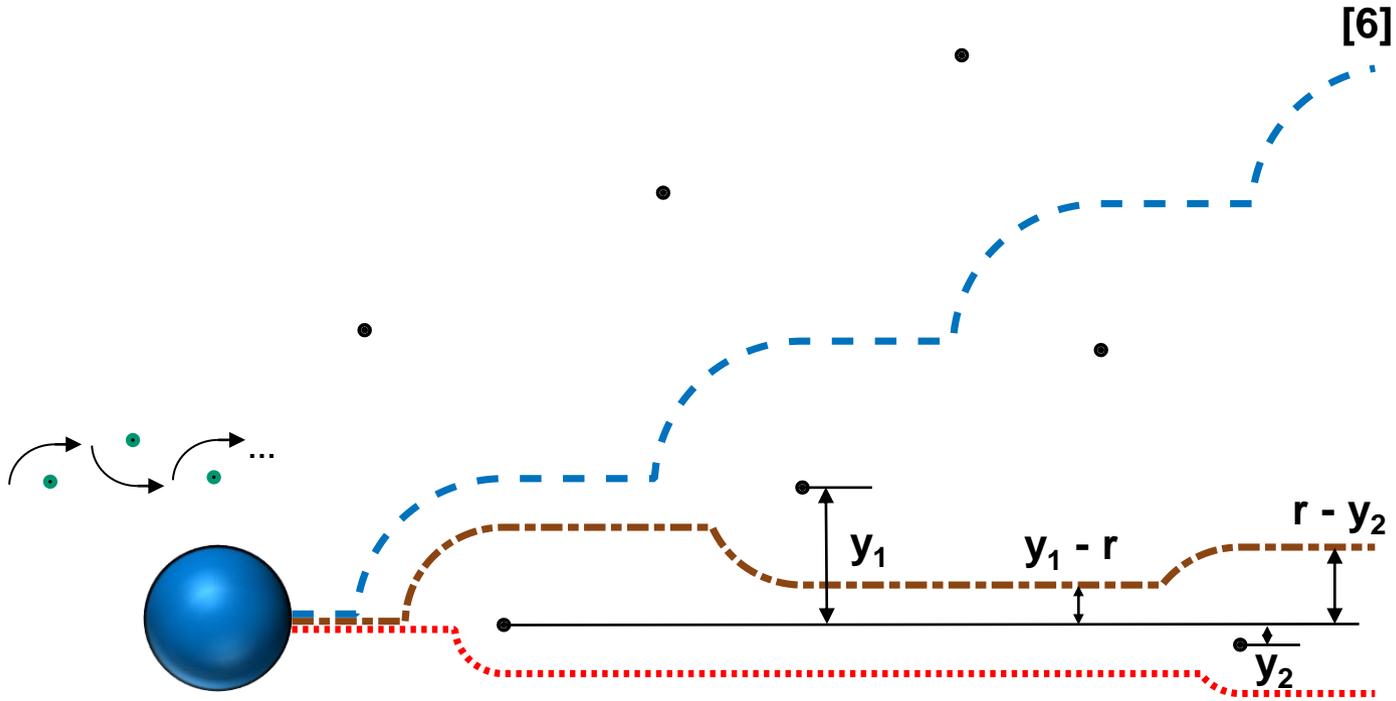
- Under what conditions does a particle follow a  ... orbit?



$r \geq |y|$

True of  ... as well!

# After determining which orbits are possible, we characterized trajectories that were previously not fully understood



**Period-2 orbit occurs**

$$\text{if } y_1 - r \leq r - y_2$$

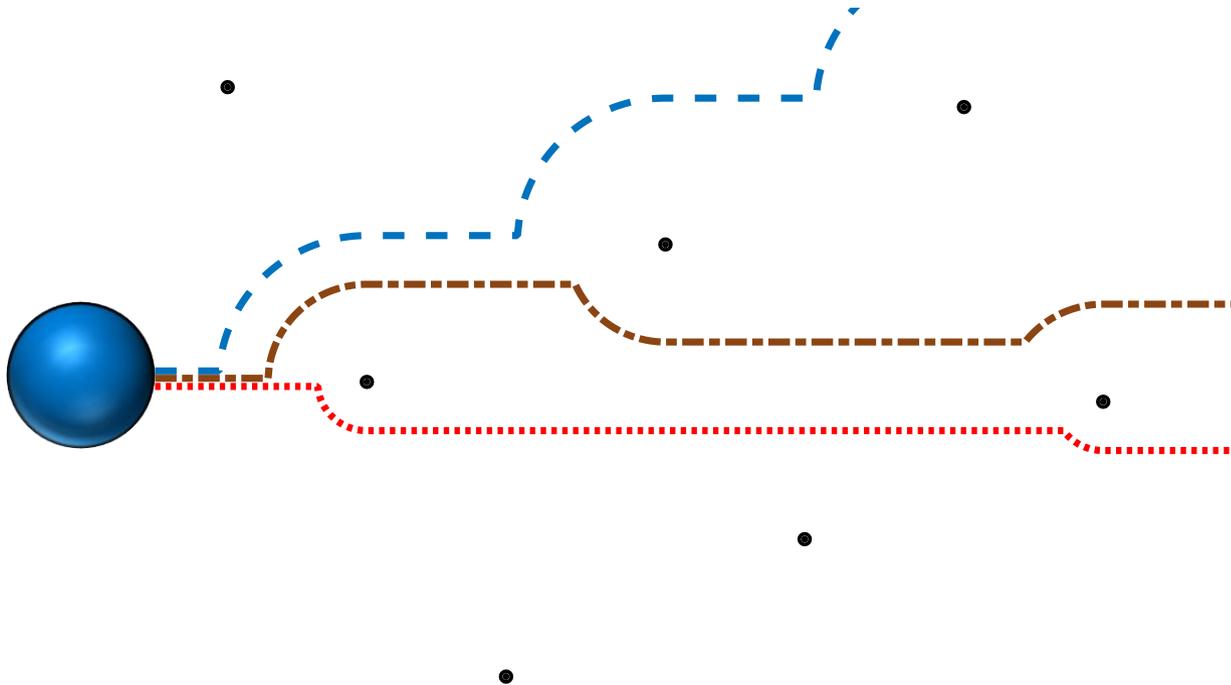
or

$$y_1 \geq r \geq \frac{y_1 + y_2}{2}$$

After determining which orbits are possible, we characterized trajectories that were previously not fully understood

[6]

As a function of particle radius, there is always a period-2 orbit sandwiched between period-1 orbits for all obstacle lattice geometries!



# We can determine the lattice coordinate where a trajectory repeats its dynamical cycle

```
Sort lattice coords. (x,y) by increasing x value
r = biggest possible value,  $y_{prev} = y$  of first obst. on list
For increasing  $x > 0$ ,
  if  $r \geq |y|$ 
    if  $r \geq \frac{|y| + |y_{prev}|}{2}$ 
      mode is period-2 ( $g = 2$ )
      next mode is period-1 on same (x,y)
    else
      mode is period-1 ( $g = 1$ )
   $y = y_{prev}$ 
  decrease r enough to not satisfy inequality
  else
    proceed to next (x,y) pair in sequence
end
```

# We can now obtain key dynamical readouts for particles displacing through lattices of this type

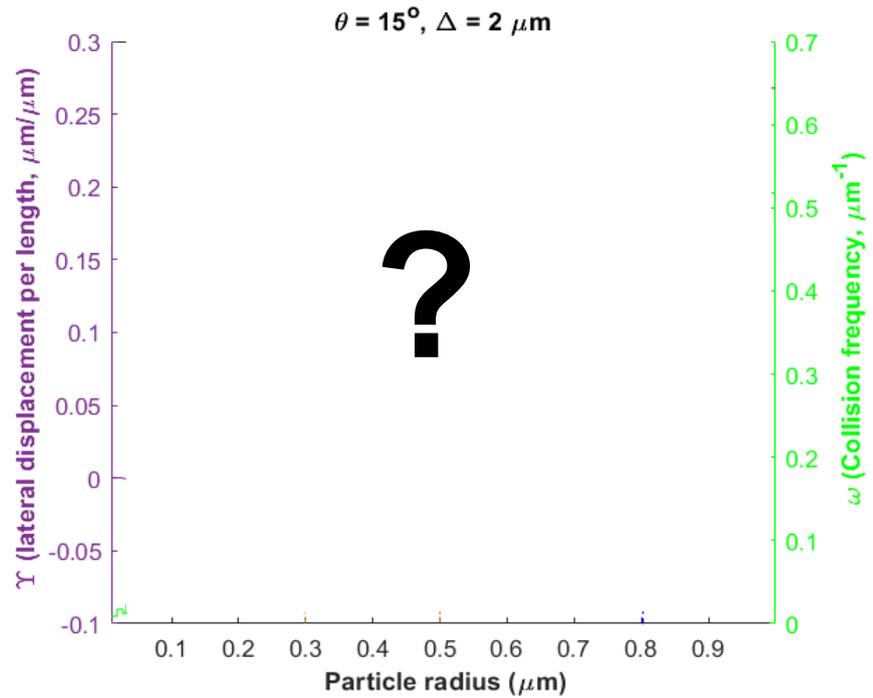
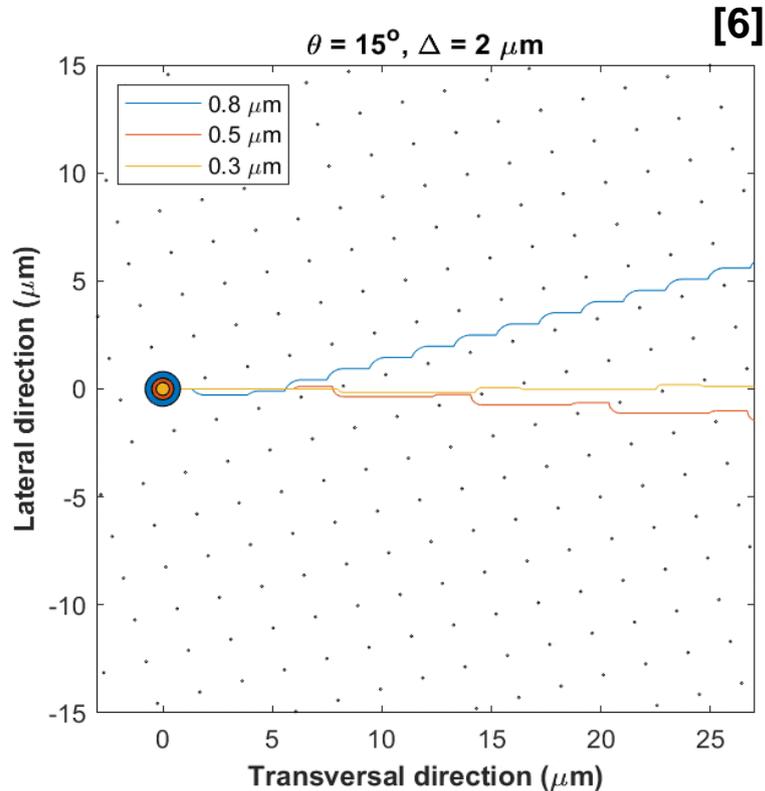
- If we average the lateral displacement and collision frequency over a single dynamical cycle:

- Lateral displacement per length =  $\frac{y}{x}$

- Spatial collision frequency =  $\frac{g}{x}$

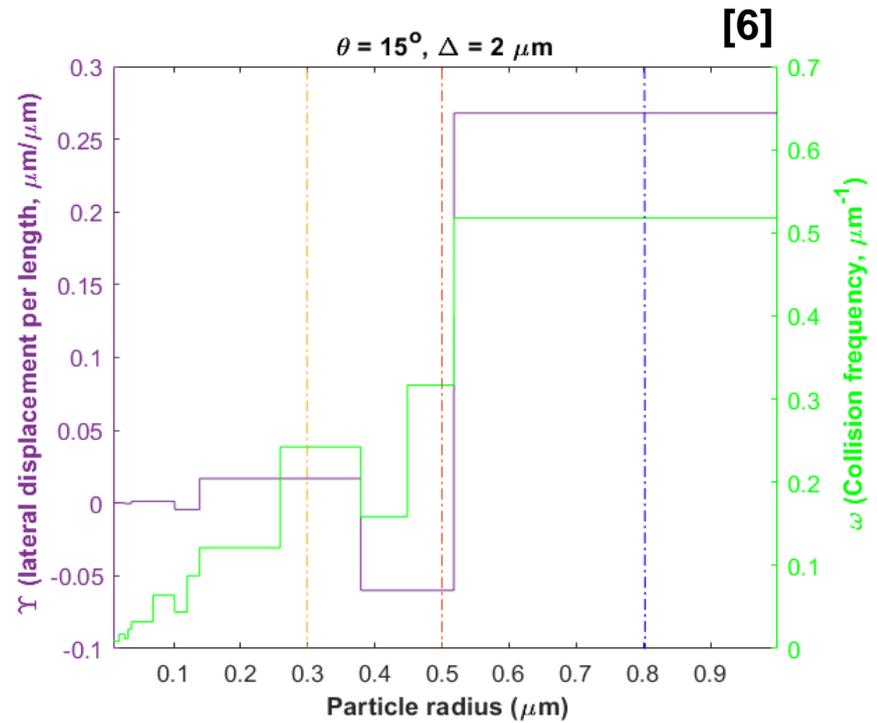
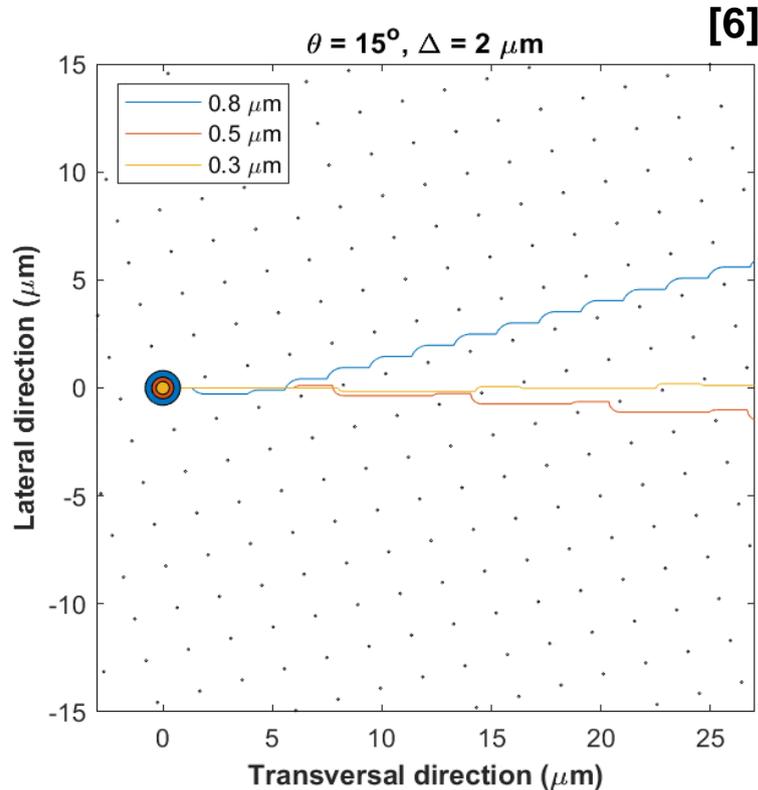
# We've used this framework to predict all possible particle trajectories through the microchannel

- Thanks to this theoretical framework, we can fully predict the trajectories a particle can take through the microfluidic lattice.



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- Thanks to this theoretical framework, we can fully predict the trajectories a particle can take through the microfluidic lattice.



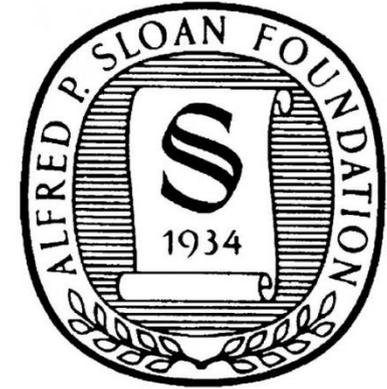
# **Work in the literature validates that we have captured the dominant physics and that the theory is extendable**

- **Our results are in good qualitative & quantitative agreement with what's been described in the literature ([3][7][8][9] among many others).**
- **Particularly, [9] discusses the existence of a parameter describing the irreversible displacement of a particle after a collision in a square lattice of finite-sized obstacles.**
  - **Incorporates finite obstacle size/hydrodynamics**
  - **Converges to  $\pm r$  in the infinitesimal obstacle limit**
  - **Could this Risbud-Drazer parameter be the key to extending this theory to finite sized obstacles?**

# Acknowledgements

## Kirby Research Group

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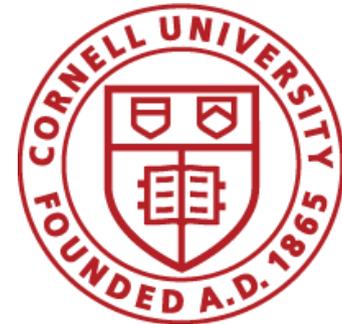


## External Collaborators

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# Understanding colloidal particle dynamics in microfluidic obstacle arrays with symbolic dynamics

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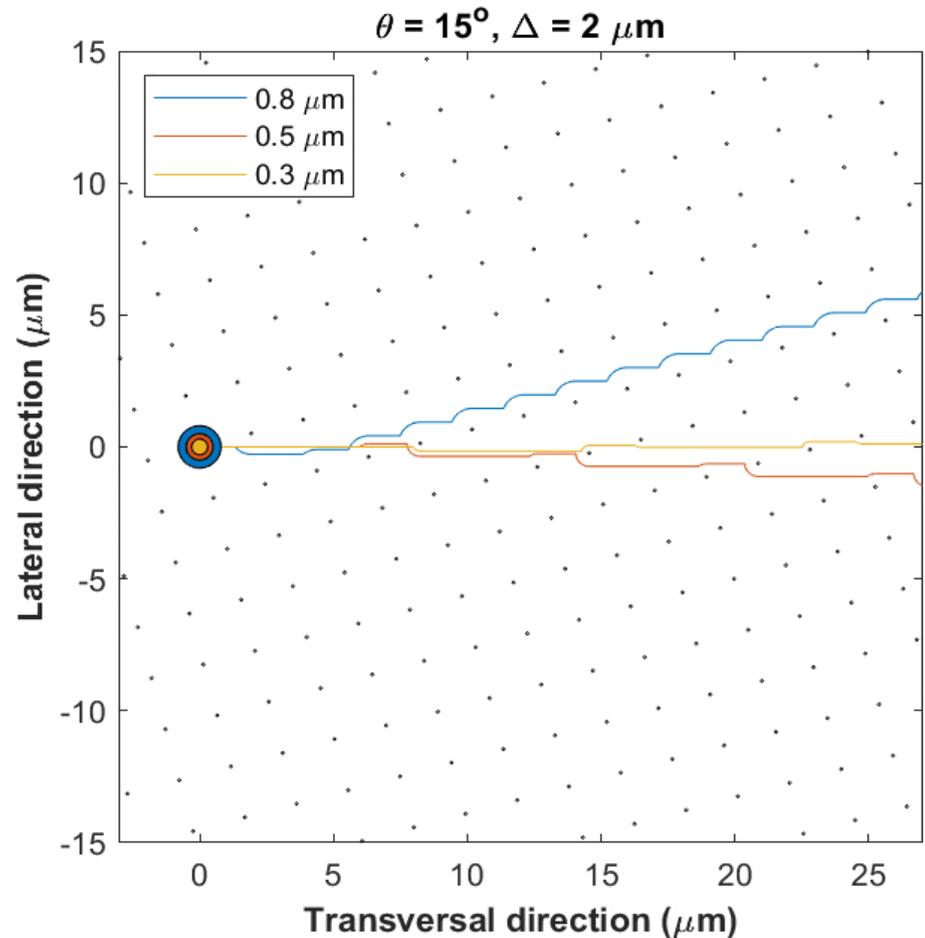
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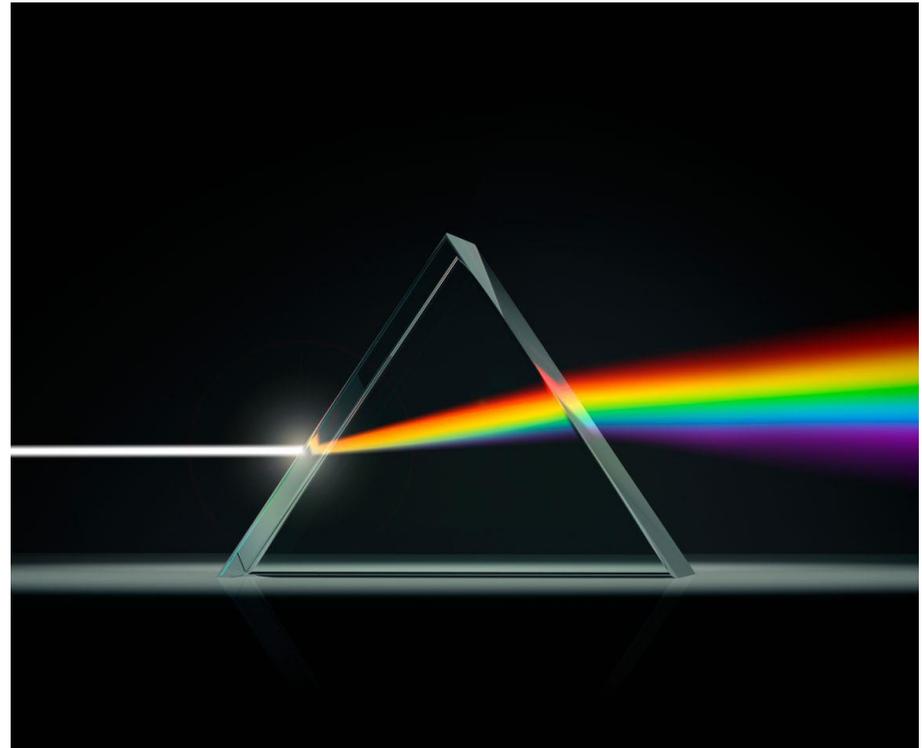
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# Chaining Obstacle Lattices Lets Us Generate Versatile Particle Sorting Microdevices

- We can chain obstacle lattices with different parameters to obtain displacement behaviors unavailable in single lattices.
- Total lateral displacement and collision number are additive.



Total lateral displacement  $\rightarrow d = \sum_{i=1}^N d_i = \sum_{i=1}^N \ell_i \gamma_i$

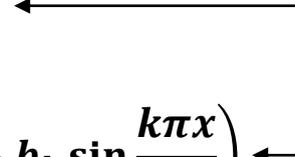
Lateral displacement per length  $\rightarrow \ell_i \gamma_i$

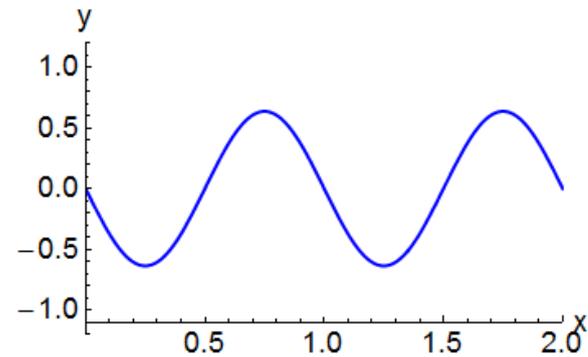
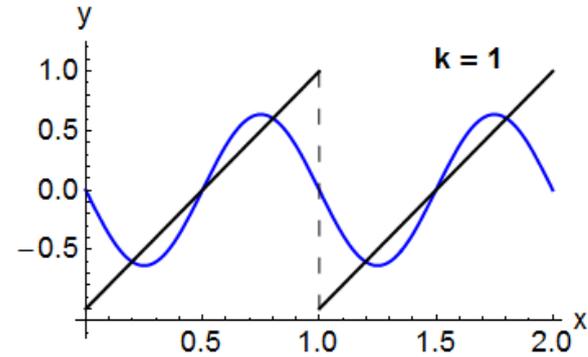
Total no. of collisions  $\rightarrow c = \sum_{i=1}^N c_i = \sum_{i=1}^N \ell_i \omega_i$

Spatial collision frequency  $\rightarrow \ell_i \omega_i$

Lattice length (streamwise)  $\rightarrow \ell_i$

# Our method of approximating target functions is very similar to Fourier series approximation

$$d(\mathbf{r}) = \sum_{i=1}^n \ell_i \Upsilon_i$$
$$f(x) = \sum_{k=0}^{\infty} \left( a_k \cos \frac{k\pi x}{L} + b_k \sin \frac{k\pi x}{L} \right)$$


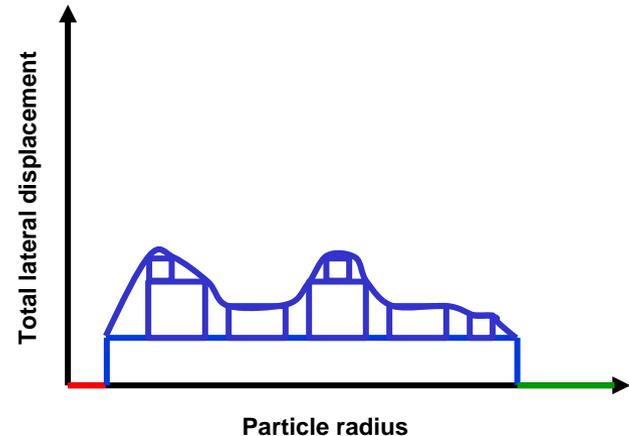
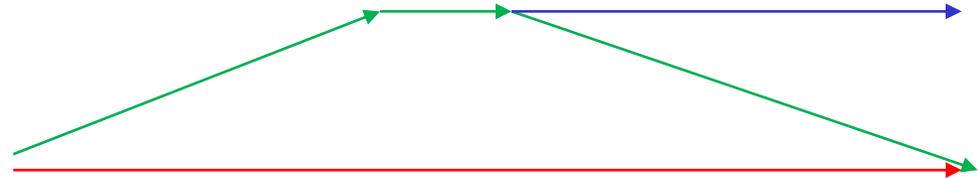


**Same mathematical structure, but  $\Upsilon_i$  are not orthonormal!**

**How do we know this kind of approximation process can always work?**

# We've shown that we can approximate any given lateral displacement function of size with chained lattices

- We *can* approximate any lateral displacement function of particle size using a sequence of specific pairs of rotated square lattices.
- The type of approximation we use is convergent with respect to many common error metrics, like least squares and least absolute deviation for both continuous and discrete functions.



# We have developed a systematic inverse design algorithm for microfluidic lattice chains

- For a chain of  $n$  lattices, we find the individual lattice parameters that best approximate some target function.
  - Lattice parameters  $\ell_i, \vec{a}_i, \vec{b}_i$   
 $\rightarrow \ell_i, \Delta_i, \theta_i$
- We approximate by sequentially increasing lattice number.
  - Lattice complexity reduced as much as possible.
  - Accuracy thresholds can be established.
  - Convergence guaranteed.

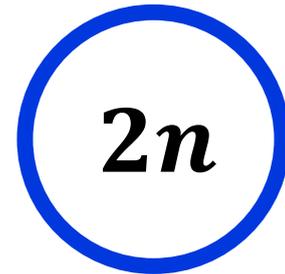
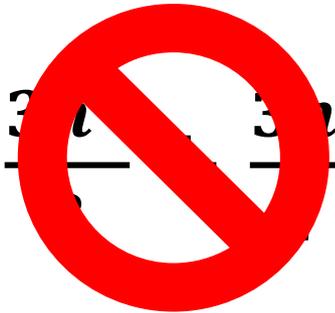
Optimization  
algorithm  
dimension:

$$\frac{3n^2}{2} + \frac{3n}{2}$$

$n$	Dimensions
1	3
2	9
3	18
4	30

# We have significantly improved dimensionality constraints by applying mathematical tools

- **Least-squares solving reduces dimensionality drastically.**
  - Hilbert projection theorem ensures sequential solutions are still global solutions.
  - Since lateral displacement is linear in lattice lengths, closed-form solutions for lengths exist given the other two parameters.



- **To ensure unique solutions, we maximize the inner product of the target function with the lateral displacement per length function when lattice length is zero.**

# To validate our designs, we utilize three different techniques and three different design metrics

## Metrics

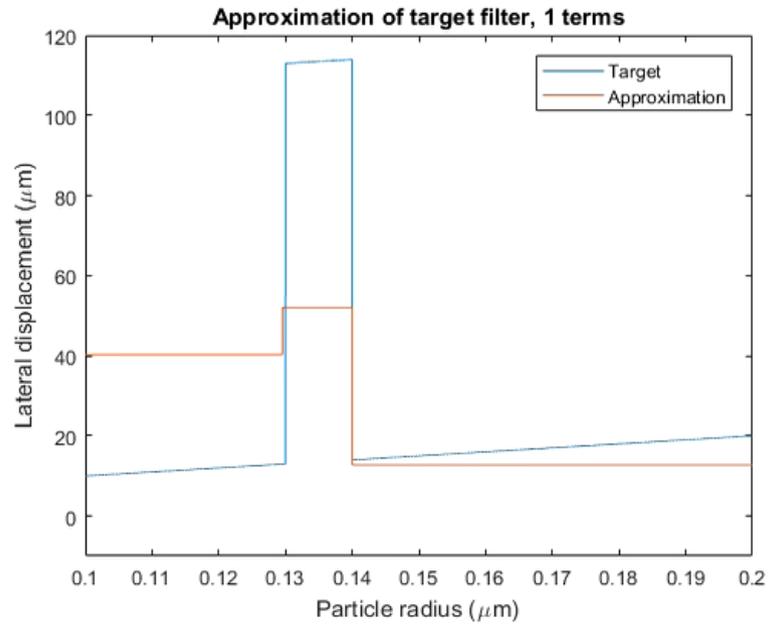
- **Device complexity (# of lattices)**
  - High complexity leads to amplification of edge effect/lock-in errors between lattices
- **Total device length**
  - Large device lengths cause lateral pressure gradients to develop, harming the DLD effect
- **Mean square error to target**
  - Large error diminishes intended device performance

## Techniques

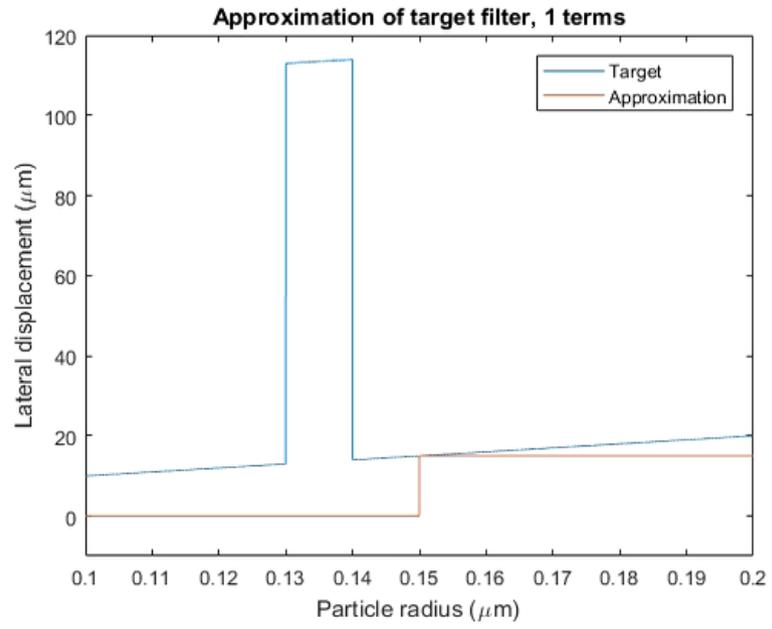
- **Direct L2**
  - Directly finds the lattice parameters that minimize the cost function with no extra constraints.
- **$\theta$ -restricted L2**
  - As above, but fixing the angle such that LD function are step functions.
- **Riemann**
  - Doesn't use optimization, fits the target with step functions. Consistent with current design strategies.

# Optimization improves error convergence considerably for nearly every target function

## Direct L2 method



## Riemann method

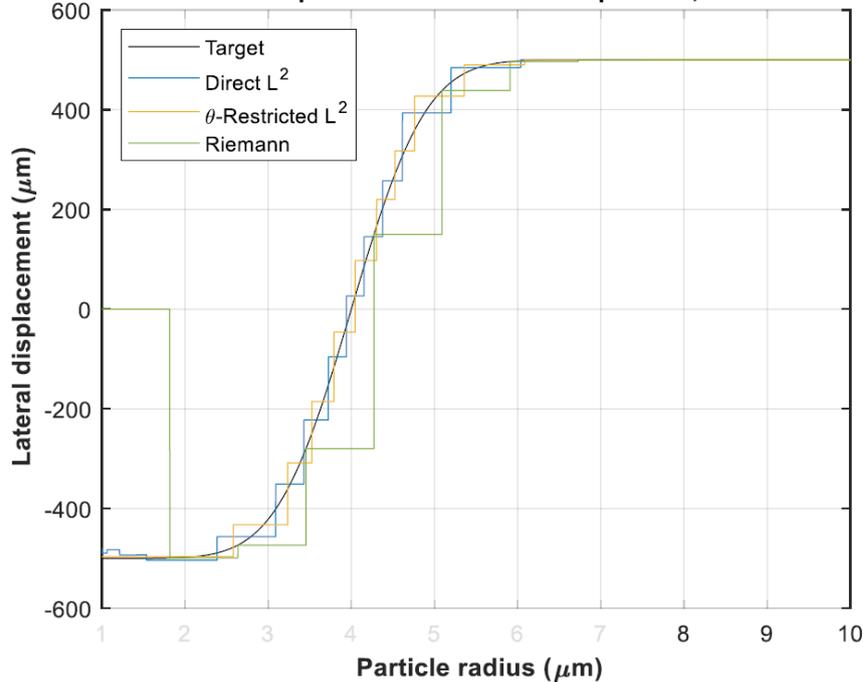


# Our algorithms are considerably better at constructing “prismatic” microdevices than the unoptimized approach

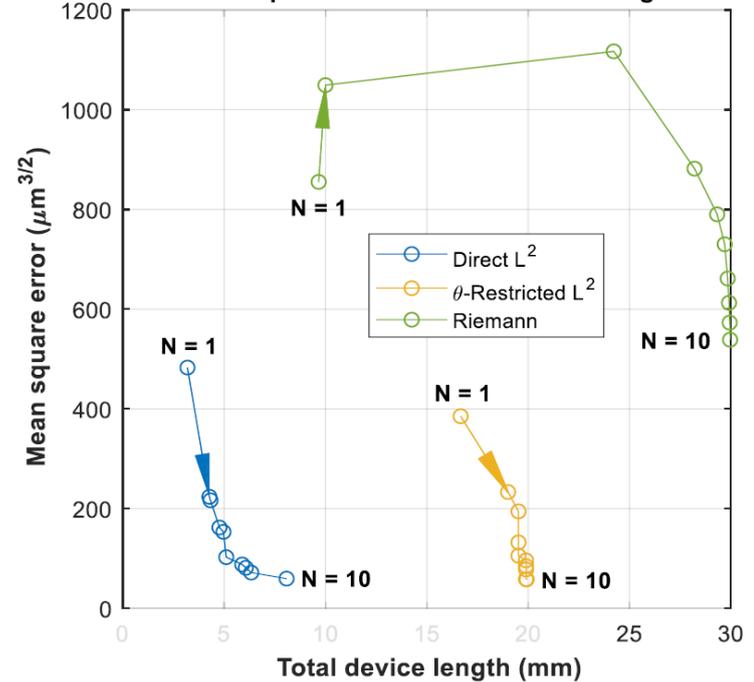


$n = 10$

Lateral displacement function comparison,  $N = 10$  [6]



Mean square error vs. total device length [6]



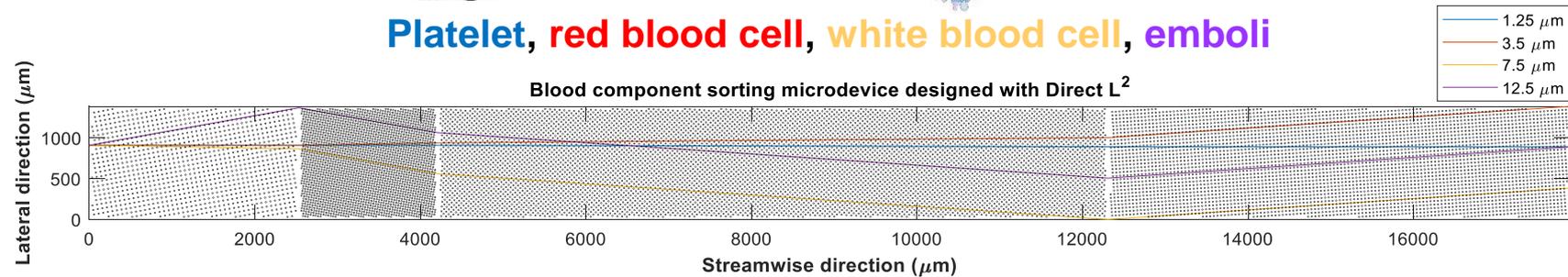
# We can use novel knowledge about these colloidal dynamics to construct devices that sort arbitrary polydisperse suspensions



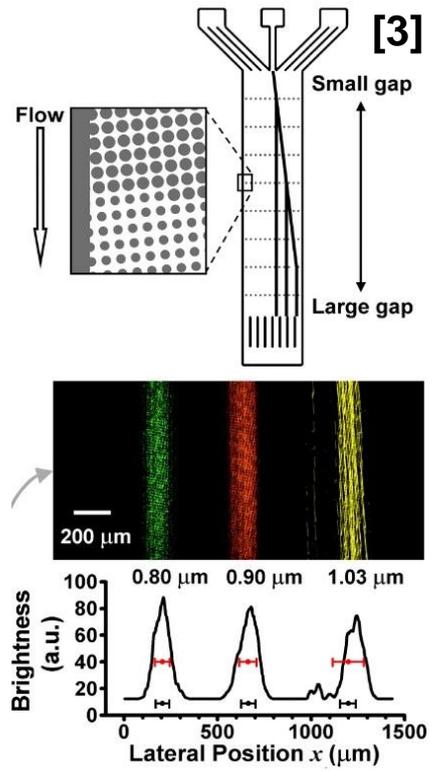
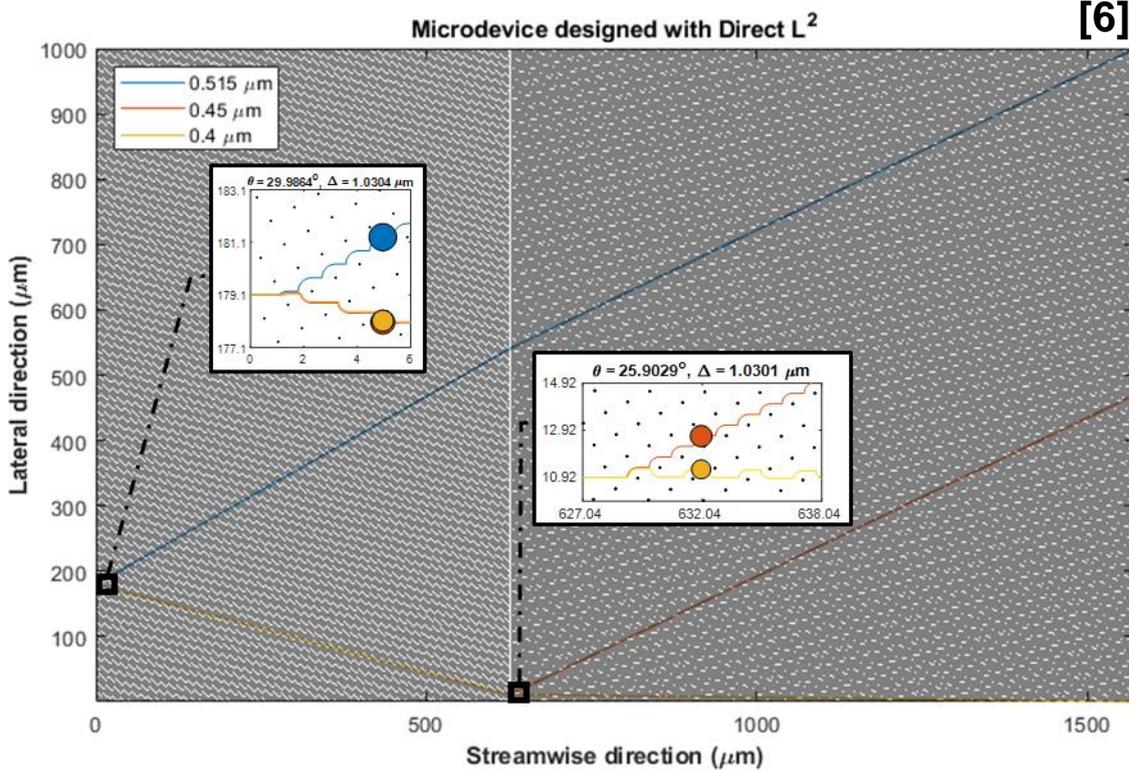
Platelet, red blood cell, white blood cell, emboli

[6]

Blood component sorting microdevice designed with Direct L<sup>2</sup>



# Our device designs vastly outperform those reported in literature, in theory



	Huang et al. (2004)	Rodriguez-Gonzalez et al. (2020)
Number of lattices	8	2
Total device length	14 mm	1.57 mm

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